

## Polymer blend: a new approach for eliminating curing effect of aqueous dispersion coatings

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The aim of present work was to investigate blends of Eudragit® NE 30D with Aquacoat® ECD using different ratios to eliminate curing effect associated with individual polymers. Propranolol HCl 10% w/w was layered onto sugar cores using 5% w/w HPMC as a binder. Drug-layered-cores were coated either with pure or blends of Aquacoat® ECD: Eudragit® NE 30D in a fluidized bed coater to obtain 20% w/w coating level. Talc 35% w/w was used as anti-tacking agent. The pellets were characterized for in vitro dissolution studies, morphology, water uptake-weight loss, osmolality and adhesion of coating after curing at 60 °C or 60 °C/75% RH for 24 h. The findings revealed that Aquacoat® ECD coated pellets showed curing effect due to further gradual coalescence of polymeric particles which resulted into better film formation upon curing. In contrast, the curing effect of Eudragit® NE 30D coated pellets was caused by decrease in adhesion of coatings after curing which provided entirely different swelling behavior of uncured (localized swelling) and cured (uniform swelling) pellets. The undesired curing effect of individual polymers was eliminated by using their blends in appropriate ratio.

**Keywords:** Aqueous dispersion coatings. Polymer blend. Coated pellets. Curing effect. Adhesion.

### INTRODUCTION

Polymeric film coatings are commonly employed onto solid dosage forms (pellets, tablets granules and capsules etc) in order to modify the drug release characteristics (Ho *et al.*, 2009; Muschert *et al.*, 2009a). These widespread film coatings are sprayed onto substrates either from organic polymer solutions or from aqueous polymer dispersions. However, the

application of aqueous polymer dispersions offers numerous advantages over organic polymer solutions such as: less environmental hazards due to avoidance of organic solvent, no flammability concerns and higher solid contents can be coated with aqueous dispersions thus reducing processing time and cost effectiveness (McGinity, Linda, 1997; Fukumori, 1997). But, care has to be taken during coating of aqueous dispersion as the film formation mechanism from these dispersions is complex. Sometimes film is not completely coalesced during coating and further gradual coalescence upon storage leads to unstable release profiles (Shao *et al.*, 2002; Muschert *et al.*, 2009b; Kolter *et al.*, 2013).

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Decrease in drug release (curing effect) upon storage has been reported in literature for commercially available dispersions such as Eudragit<sup>®</sup> RS and RL 30D, Surelease<sup>®</sup> and Aquacoat<sup>®</sup> ECD (Dashevsky *et al.*, 2005; Siepmann *et al.*, 2007). This is due to high minimum film forming temperature (MFT) of these polymers that could cause incomplete coalescence of colloidal polymer particles during coating process.

Different process and formulation parameters (e.g., coating thickness, concentration of polymer and type, and amount of added plasticizer) are varied in order to achieve a desired drug release pattern. However, these variations are often difficult to apply due to not formation of appropriate film and also non-feasibility of processing at large scale. For example, plasticizers added in higher concentrations provide too sticky coatings whereas their lower concentrations result into fragile and brittle films (Siepmann *et al.*, 2005; Siepmann *et al.*, 2008). To overcome such problems, a potential approach is to use the blend of two polymers which are non-toxic and exhibit different physicochemical properties (Dashevsky, Kolter, Bodmeier, 2004; Strübing, Metz, Mäder, 2007). The use of polymer blends helps to provide broad range of drug release patterns by changing the coating properties (Lecomte *et al.*, 2005; El-Malah, Nazzal, 2008). In the case of aqueous polymer dispersions, the use of polymer blends not only helpful in reducing tackiness problems during coating process and storage but it also significantly improves long term stability of coated dosage forms by avoiding unwanted change in drug release profile upon storage (Zheng, McGinity, 2003; Kucera *et al.*, 2008). Additionally, the adhesion of coating to the substrates is improved by adding a second polymer to the coatings which is critical for avoiding curing effect (Felton, McGinity, 1999; Irfan *et al.*, 2009; Irfan *et al.*, 2017).

Eudragit<sup>®</sup> NE 30D is an ethyl methacrylate and methyl methacrylate based aqueous dispersion having a low glass transition temperature (T<sub>g</sub>) -8 °C and a minimum film forming temperature (MFT) of 5 °C. The films formed by this polymer are highly flexible and soft and therefore no plasticizer addition is recommended for coating process. Despite of its good flexibility, curing effect has been reported in literature with Eudragit<sup>®</sup> NE 30D coated dosage forms. In contrast, Aquacoat<sup>®</sup> ECD is an ethylcellulose based aqueous dispersion with T<sub>g</sub> and MFT of 135 °C and 75 °C, respectively, which results into extremely brittle films and addition of appropriate plasticizer is necessary before coating.

The stability issues of coated substrates from Aquacoat<sup>®</sup> ECD dispersion is also described in literature.

Therefore, the key objectives of this work were to investigate the blends of Eudragit<sup>®</sup> NE 30D (a polymer having low T<sub>g</sub>) with Aquacoat<sup>®</sup> ECD (a polymer with high T<sub>g</sub>) in different ratios in order to eliminate the curing effect associated with the individual polymers and to develop coating with stable drug release profiles by selecting the appropriate polymer blend ratio.

## MATERIAL AND METHODS

### Material

An aqueous dispersion of ethyl cellulose (Aquacoat<sup>®</sup> ECD) was donated by FMC, Biopolymers, Brussels, Belgium. Aqueous copolymer dispersion of ethyl acrylate and methyl methacrylate (Eudragit<sup>®</sup> NE 30D) was purchased from Evonik, Darmstadt, Germany. Sugar cores (Suglets<sup>®</sup>, 710-850 µm) were generously gifted by NP Pharma, Bazainville, France. propranolol HCl (C<sub>s</sub> = 212 mg/mL) was obtained from BASF, Ludwigshafen, Germany. Talc was purchased from Luzenac Toulouse, France. Colloidal silica (Aerosil<sup>®</sup> 200) was gifted by Evonik, Germany and triethyl citrate (TEC) was donated by Morflex, Greensboro, NC, USA.

### Drug layering of sugar cores

The model drug, propranolol HCl (10% w/w, based on cores), was layered onto sugar cores using hydroxypropyl methylcellulose (5% w/w, based on drug) as a drug binding agent. The drug layering solution was prepared in the mixture of ethanol:water (60:40) with 15% w/w solids content which was then layered onto sugar cores in a lab scale fluidized bed coater to obtain a 10% w/w drug loading

The drug layering conditions were as follows: batch size = 900 g, inlet temperature = 55 °C, airflow = 100 m<sup>3</sup>/h, product temperature = 40 ± 2 °C, nozzle diameter = 1.2 mm, atomizing pressure = 1.2 bar, spraying rate = 9 g/min. Finally, the drug-layered-cores were dried at 40 °C for 30 min

### Polymer coating of drug-layered cores

The prepared drug layered cores were coated either with pure Eudragit<sup>®</sup> NE 30D and Aquacoat<sup>®</sup> ECD or with the blends of Aquacoat<sup>®</sup> ECD: Eudragit<sup>®</sup> NE 30D (95:5,

85:15, 75:25, 60:40) using 15% w/v solids content in a lab scale fluidized bed coater (Mini-Glatt, Glatt GmbH, Binzen, Germany) to obtain 20% w/w coating level (based on solid polymer weight). In order to avoid sticking during coating process, talc 35% w/w (based on solid polymer weight) was added in all investigated coatings. In the case of coating with pure Aquacoat® ECD, 25% w/w triethylcitrate (TEC) (based on solid polymer weight) was added to coating dispersion for plasticization whereas no plasticizer was added to Eudragit® NE 30D. Optionally, the pure Aquacoat® ECD was also coated without adding plasticizer. The coating process carried out with following parameters: batch size = 50 g, inlet temperature = 45 °C, product temperature = 38-40 °C, nozzle diameter = 0.5 mm, airflow = 0.8 m<sup>3</sup>/h, atomizing pressure = 0.2 bar, maximum spraying rate = 1 g/min, final drying of coated pellets for 10 min at 40 °C, (except for pure Eudragit® NE 30D coatings, the product temperature was adjusted to 18 °C). In order to prevent sticking during storage, the coated pellets were shaken manually with approximately 0.5% w/w of colloidal silica. The curing of coated pellets was performed at 60 °C and 60 °C/75% RH for 24 h following equilibration in a desiccator for 24 h

### Water uptake and weight loss of coated pellets

500 mg of the both uncured and cured coated pellets were precisely weighed (Initial weight), transferred into 900 mL of pre-heated 0.01 N HCl and stirred at 100 rpm at 37 ± 0.5 °C for desired time using USP apparatus II (Vankel Industries, Edison, New Jersey, USA). All samples were run in triplicate. The pellets were collected at pre-defined timer points, filtered and blotted carefully and weighed again (Wet weight). The wet filtered pellets were placed in an oven pre-set at 105 °C for 4 h and further equilibrated in a desiccator for 24 h and weighed again (Dry weight). The water uptake / weight loss were calculated using following formulae: Water uptake (%) = (Wet weight – Dry weight)/Dry weight\*100, Weight loss (%) = (Initial weight – Dry weight)/Initial weight \*100.

### In vitro dissolution studies and swelling of pellets

Drug release studies were carried out with approximately 500 ± 5 mg of coated uncured and cured pellets using USP apparatus II (Vankel Industries, New Jersey, USA). 900 mL 0.01 N HCl was selected as dissolution media at 37 ± 0.5 °C. The speed of paddles

was adjusted at 100 rpm and all samples were run in triplicate. At pre-defined intervals, samples were withdrawn and analyzed on a UV-spectrophotometer (Shimadzu UV-2101PC UV-Vis Shimadzu Europe, Duisburg, Germany).

The behavior of both uncured and cured coated pellets, while conducting dissolution studies, was recorded under a light microscope using a special software namely image analyzing software (Inteq® Informationstechnik, GmbH, Berlin, Germany). In order to estimate swelling of pellets during dissolution, the diameter of 30 pellets was measured at pre-determined time intervals. Finally, the swelling of pellets was determined using the following formula: Swelling % = (Wet volume – Dry volume)/Dry volume\*100

### Morphology of pellets

In order to observe swelling behaviour during drug release, the pellets approximately 100 mg were placed into 0.01 N HCl in a small Petri dish at 37 °C, the pictures were taken after pre-defined intervals with the help of an image capturing software which were also converted into videos. Additionally, the macroscopic pictures of coated uncured and cured pellets before and after drug release studies were captured using a light microscope.

### Determination of adhesive force of coatings

The model tablets were formulated exactly of same composition like coated pellets and were used to determine the detachment force of the coatings to the drug-layered-cores. For that purpose, the coating of tablets was punch-cut to create a circle of around 7 mm diameter in the centre. This cut circular part of coating was attached to the metal probe of a TA.XTplus Texture Analyzer (Stable Micro Systems, Godalming, England) with the help of strong adhesive tape. The force at which coating separated from the rest of core was recorded as maximum adhesive force (n = 6).

### Preparation of free films

The free films were prepared with the help of a casting knife, using aqueous polymer dispersion exactly of same compositions that were used for the pellet coatings, in small petri dishes. The films were dried at ambient condition, peeled off, packed in air tight polythene bags and stored in desiccator until further use.

## Differential scanning calorimetry (DSC)

The casted films were used for performing DSC studies with the help of a DSC 821e (Mettler-Toledo GmbH, Gießen, Germany). Samples approximately 8–10 mg were weighed and enclosed in 40  $\mu$ l crucibles pans. DSC thermograms were recorded applying 10 K/min heating rate from -20 to 150  $^{\circ}$ C for all the investigated films with 80 mL/min flow rate of N<sub>2</sub> gas. The computed extrapolated peaks were used to estimate T<sub>g</sub> using the Starw Software (Mettler-Toledo GmbH, Gießen, Germany).

## RESULT AND DISCUSSION

Curing effect (decrease in drug release) is one of the most critical challenges associated with the use of aqueous polymer dispersions for developing oral controlled release dosage forms (tablets, pellets and granules etc) as described in literature (Hudovornik, Vrečer, 2015; Cuppoka *et al.*, 2011; Kranza, Gutsche, 2009). Eudragit<sup>®</sup> NE 30D is a flexible whereas Aquacoat<sup>®</sup> ECD is a brittle polymer and curing effect has been reported with both of these polymers, despite of their entirely different mechanical behavior, without providing clear mechanistic understandings. Therefore, this work was an effort to explain what could be the reasons for the curing effect of Eudragit<sup>®</sup> NE 30D and Aquacoat<sup>®</sup> ECD coatings, also if their polymer blend could be a promising approach to eliminate curing effect and to develop formulations with stable release profile.

A clear difference in drug release rates of uncured and cured Eudragit<sup>®</sup> NE 30D (Figure 1B) and Aquacoat<sup>®</sup> ECD (Figure 1A) coated pellets showed a strong cured effect which was more profound at elevated temperature and humidity.

The results of supportive studies such as water uptake, weight loss and swelling of Eudragit<sup>®</sup> NE 30D and Aquacoat<sup>®</sup> ECD coated pellets were as follows: for instance, the water uptake and swelling of Aquacoat<sup>®</sup> ECD coated pellets did not change upon curing (Figure 2A, 2C) whereas the weight loss of uncured and cured Aquacoat<sup>®</sup> coated pellets was in adherence with the drug release (Figure 2B).

The unchanged swelling of both uncured and cured Aquacoat<sup>®</sup> ECD coated pellets was also supported by observing no visible change in macroscopic pictures of the uncured and cured pellets after drug release (Figure 4). In contrast, the Eudragit<sup>®</sup> NE 30D coated cured

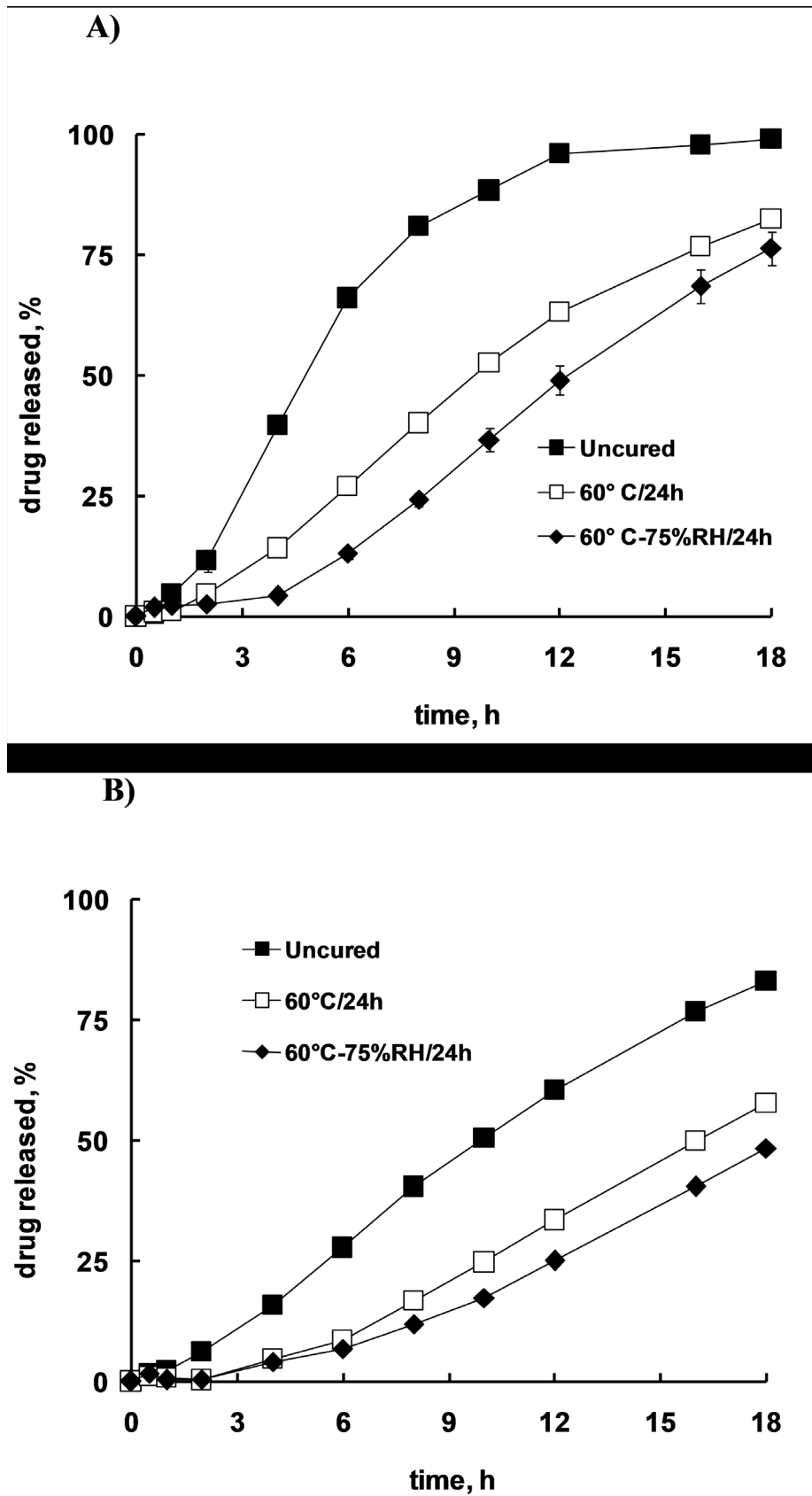
pellets revealed increased water uptake and swelling in comparison to the uncured ones (Figure 2D, 2F), which could also be confirmed from the macroscopic pictures after drug release of the uncured and cured pellets wherein a noticeable increase in pellet size was seen after curing (Figure 5). However, the weight loss of uncured and cured Eudragit<sup>®</sup> NE 30D coated pellets was in connection with released drug. For instance, the higher weight loss of uncured pellet was balanced by faster drug release and vice versa (Figure 3E)

Moreover, the video monitoring during dissolution of the uncured and cured Aquacoat<sup>®</sup> ECD coated pellets did not provide any notable difference in the swelling behavior (Figure 4A-F).

In comparison, the Eudragit<sup>®</sup> NE 30D coated uncured and cured pellets revealed entirely disparate swelling behavior during video monitoring. In the case of uncured pellets, localized swelling of the coating was observed whereas the coating of cured pellets was uniformly and extensively swollen, as a result, the cured pellets were significantly larger in size when compared to the uncured pellets (Figure 5A-F) (Irfan *et al.*, 2009; Irfan *et al.*, 2017; Dashevsky *et al.*, 2010).

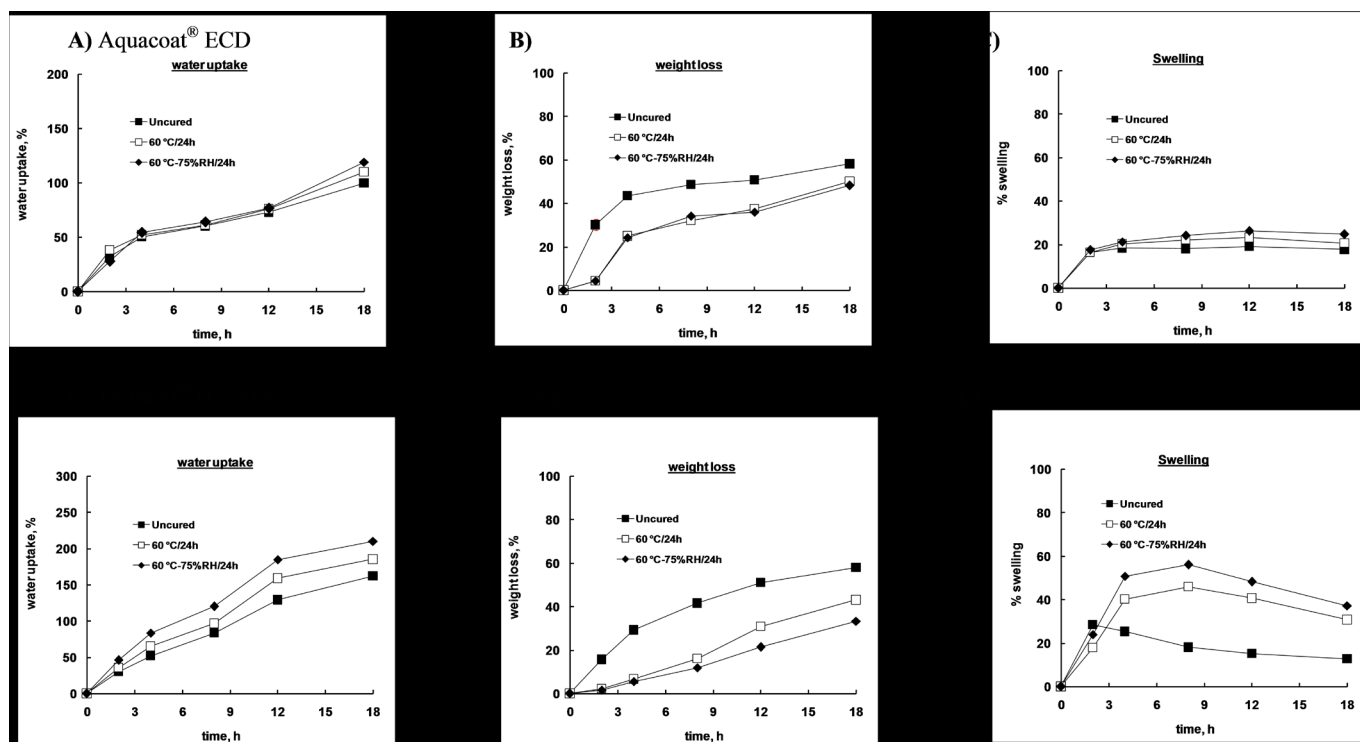
With respect the adhesive force of the coating, determined using model tablets, it was found that to Aquacoat<sup>®</sup> ECD coatings was not significantly altered after curing (Figure 6A) and, after taken out of the stability chamber (60  $^{\circ}$ C-75% RH), they were not sticky and wet upon feeling. However, the adhesive force of Eudragit<sup>®</sup> NE 30D coatings was decreased upon curing (Figure 6B), and interestingly, they were sticky and wet when taken out of stability chamber at 60  $^{\circ}$ C-75%RH. The decreased adhesive force of Eudragit<sup>®</sup> NE 30D coating could be due to breaking of interfacial bonding caused by water penetration through to the coatings and also by changed swelling coefficient of core and coating (Felton, McGinity, 1999; Irfan *et al.*, 2009; Irfan *et al.*, 2017). This could also be the reason for extensive uniform swelling of cured Eudragit<sup>®</sup> NE 30D coated pellets.

Differences in behavior in the dissolution tests observed between the two polymers can be attributed to differences in their mechanical properties. Aquacoat<sup>®</sup> ECD produces better coalescence of the particles and formation of more cohesive and stable films, even after storage under drastic conditions; on the other hand, films obtained with Eudragit<sup>®</sup> NE 30D presented a reduction of adhesive strength to the nuclei, with swelling, both for cured and uncured pellets, and consequent increase in the release time (Irfan *et al.*, 2017).

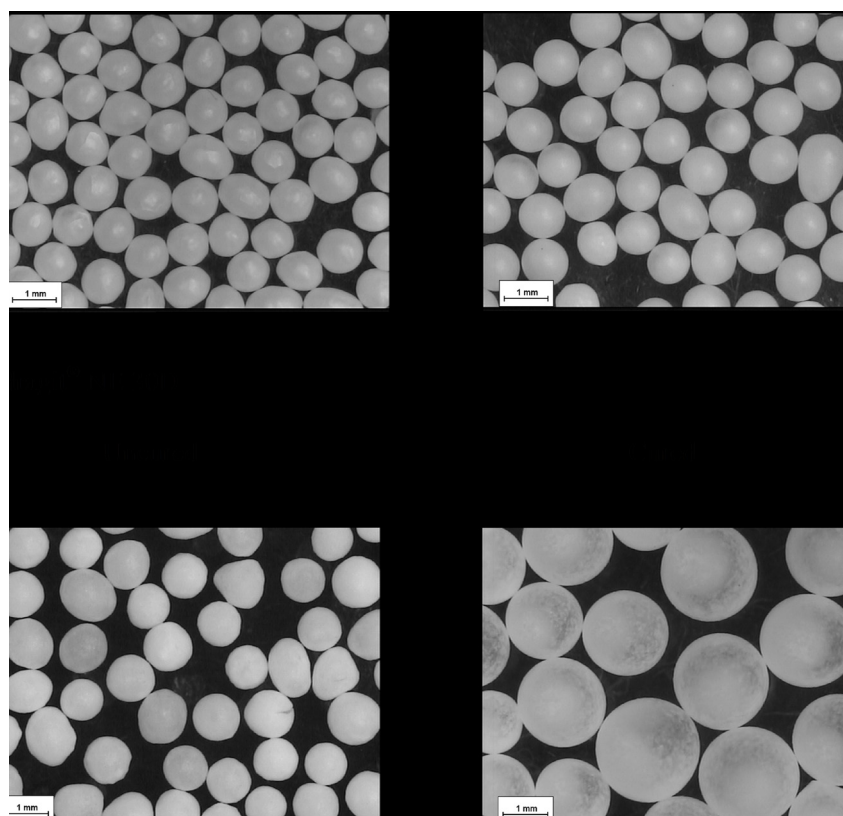


**FIGURE 1** - Effect of curing on drug release from pellets based on sugar cores loaded with 10% propranolol HCl and coated with: **A)** Aquacoat® ECD using TEC 25% and Talc 35%, **B)** Eudragit® NE 30D using Talc 35%, coating level 20%.

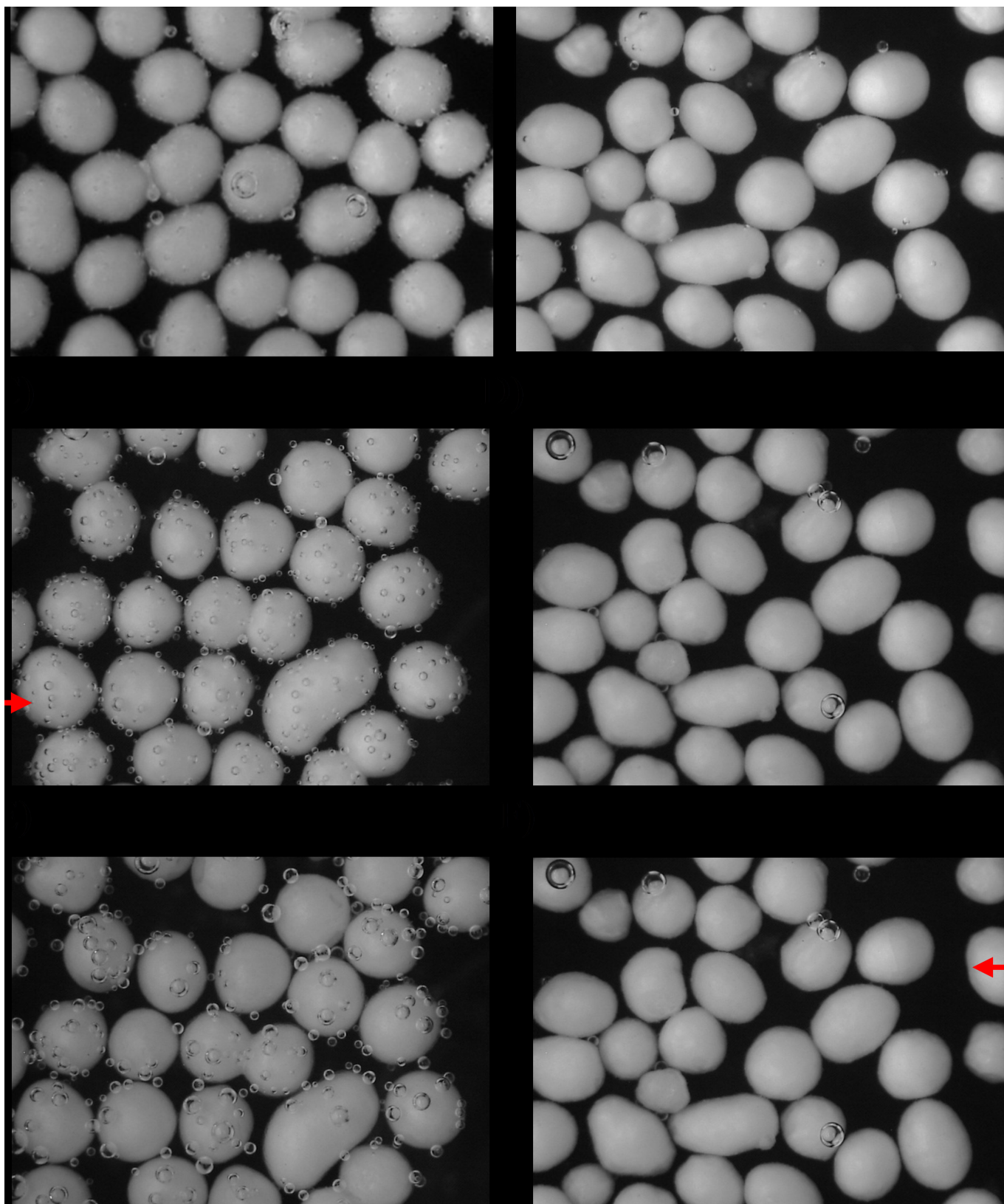




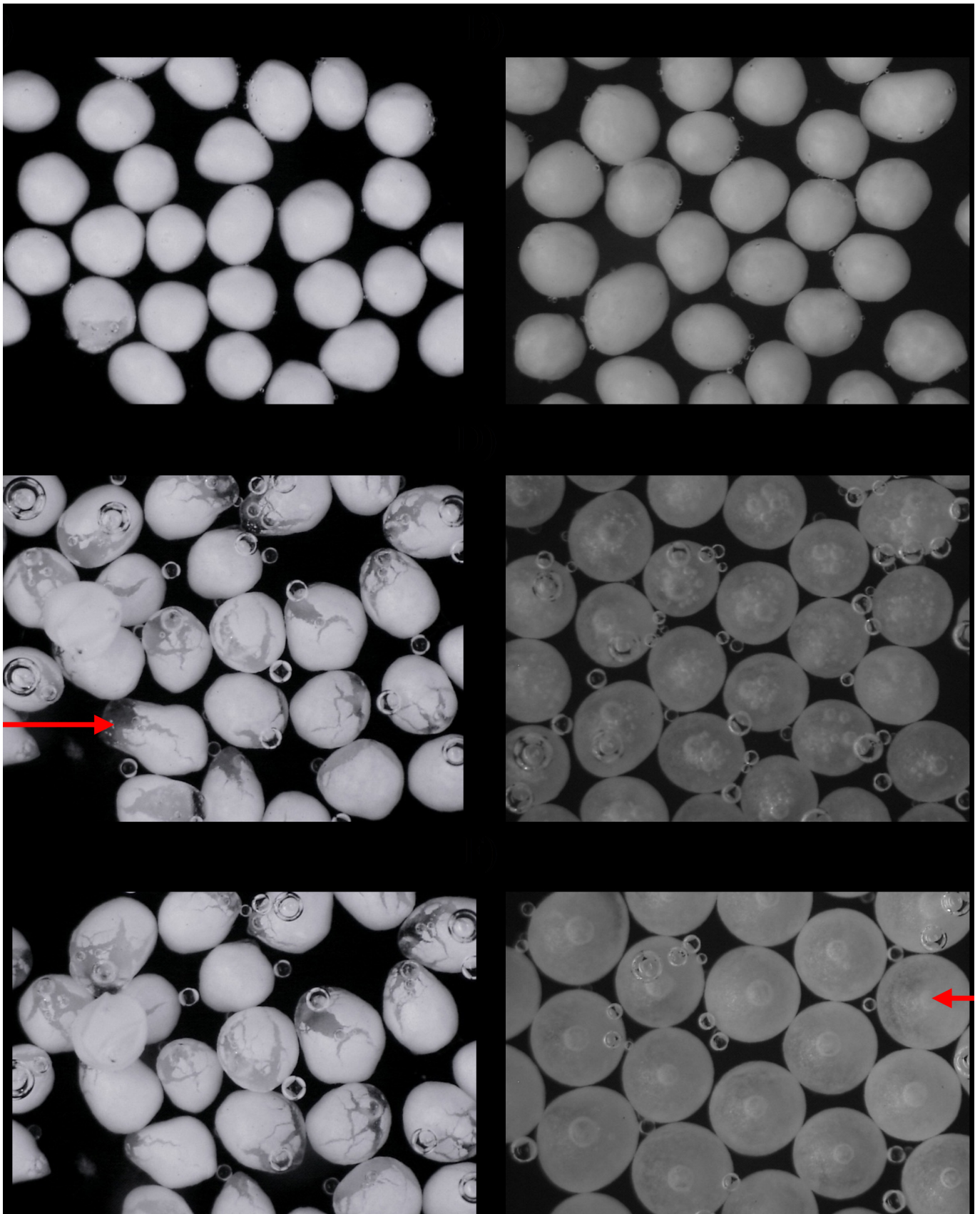
**FIGURE 2** - Water uptake-weight loss and swelling of uncured and cured pellets as a function of time in 0.01 N HCl based on sugar cores loaded with 10% propranolol HCl and coated with: **A-C)** Aquacoat<sup>®</sup> ECD and **D-F)** Eudragit<sup>®</sup> NE 30D, coating level 20%.



**FIGURE 3** - Macroscopic pictures of uncured and cured (60 °C/75% RH/24 h) coated pellets based on sugar cores loaded with 10% propranolol HCl after drug release in 0.01 N HCl: **A)** Aquacoat<sup>®</sup> ECD and **B)** Eudragit<sup>®</sup> NE 30D.

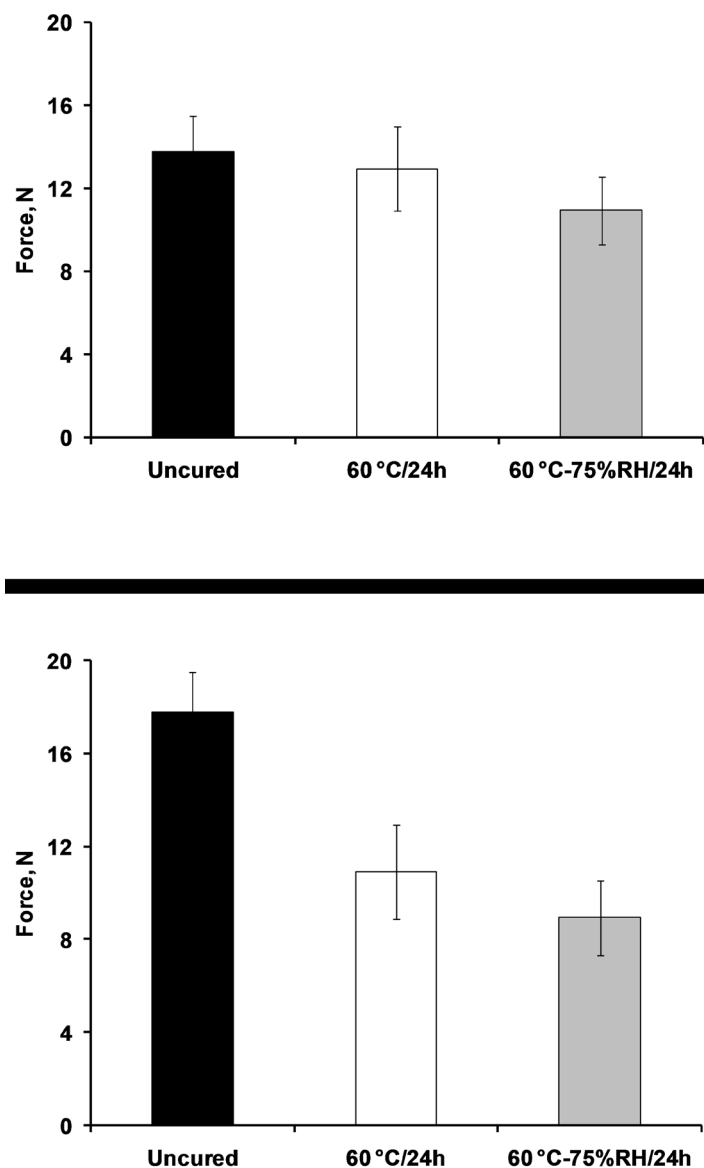


**FIGURE 4** - Macroscopic pictures of uncured and cured (60 °C/75% RH/24 h) pellets based on sugar cores loaded with 10% propranolol HCl coated with Aquacoat® ECD using talc 35% as a function of time in 0.01 N HCl.



**FIGURE 5** - Macroscopic pictures of uncured and cured (60 °C/75% RH/24 h) pellets based on sugar cores loaded with 10% propranolol HCl coated with Eudragit® NE 30D using 35% talc as a function of time in 0.01 N HCl.





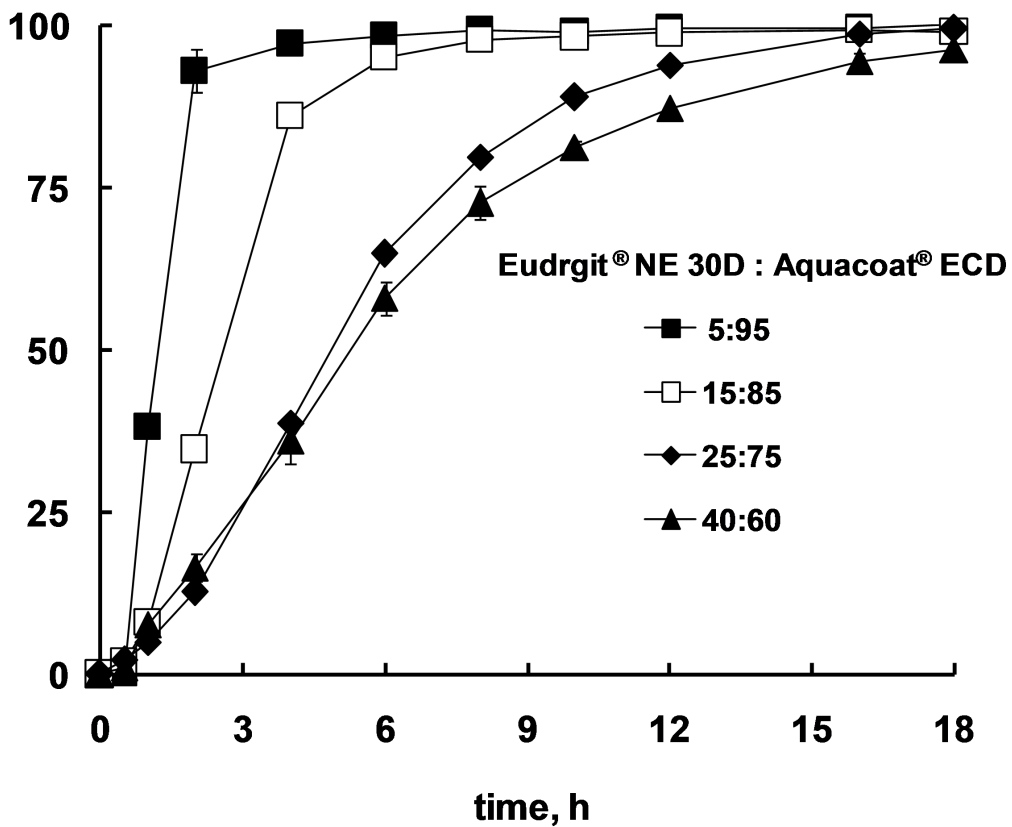
**FIGURE 6** - Effect of curing on adhesive force of polymeric coatings to the drug-layered-cores using model tablets (drug layered and polymer coated like pellets): **A)** Aquacoat® ECD and **B)** Eudragit® NE 30D, coating level 20%.

To overcome curing effect associated with individual Aquacoat® ECD and Eudragit® NE 30D coatings, a new approach using blend of Eudragit® NE 30D and Aquacoat® ECD in various ratios was further investigated. The results revealed that the drug was released quickly when 5:95 (Eudragit® NE 30D: Aquacoat® ECD) blend was used, however, by increasing the Eudragit® NE 30D concentration to 25:75 (Eudragit® NE 30D: Aquacoat® ECD), the drug was released in a controlled way following sigmoidal shape of curve (Figure 7). No significant change in drug release pattern was noticed when Eudragit® NE 30D concentration

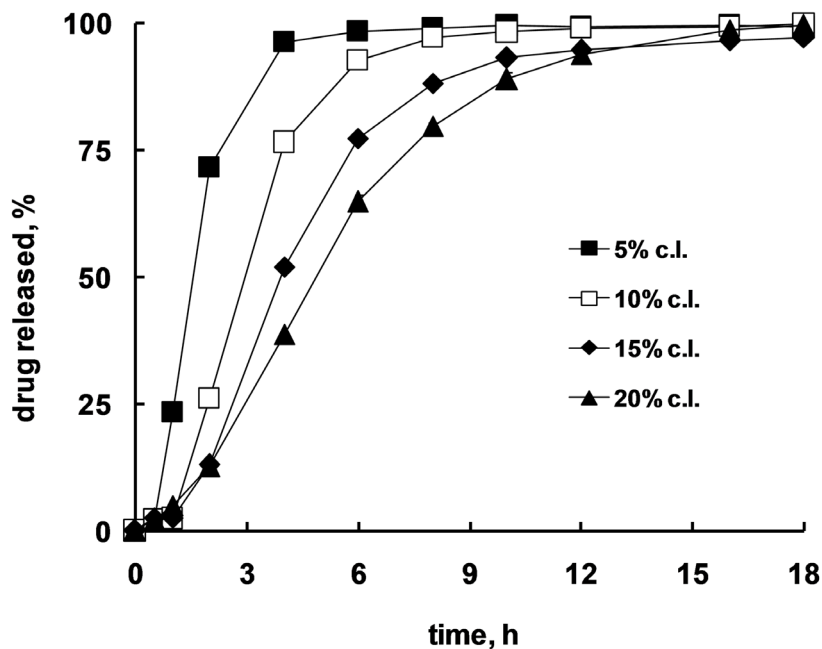
was further increased to 40:60 (Eudragit® NE 30D: Aquacoat® ECD). Therefore, in order to elucidate curing effect, the blend of Eudragit® NE 30D: Aquacoat® ECD in 25:75 ratio was used for further studies.

Figure 8 shows drug release from pellets coated using Eudragit® NE 30D: Aquacoat® ECD (25:75) at different coating levels; the drug release was decreased as a function of increasing coating level.

The water uptake-weight loss as well as swelling of the uncured and cured pellets were almost similar (Figure 10A-C).



**FIGURE 7** - Drug release from pellets based on sugar cores loaded with 10% propranolol HCl and coated with different polymer blend ratios of Eudragit® NE 30D: Aquacoat® ECD using 35% talc, coating level 20%.



**FIGURE 8** - Effect of coating levels on drug release from pellets based on sugar cores loaded with 10% propranolol HCl and coated with a polymer blend of Eudragit® NE 30D: Aquacoat® ECD (25:75) using 35% talc.

The release profile was maintained even after storage under drastic conditions of temperature and humidity (Figure 9).

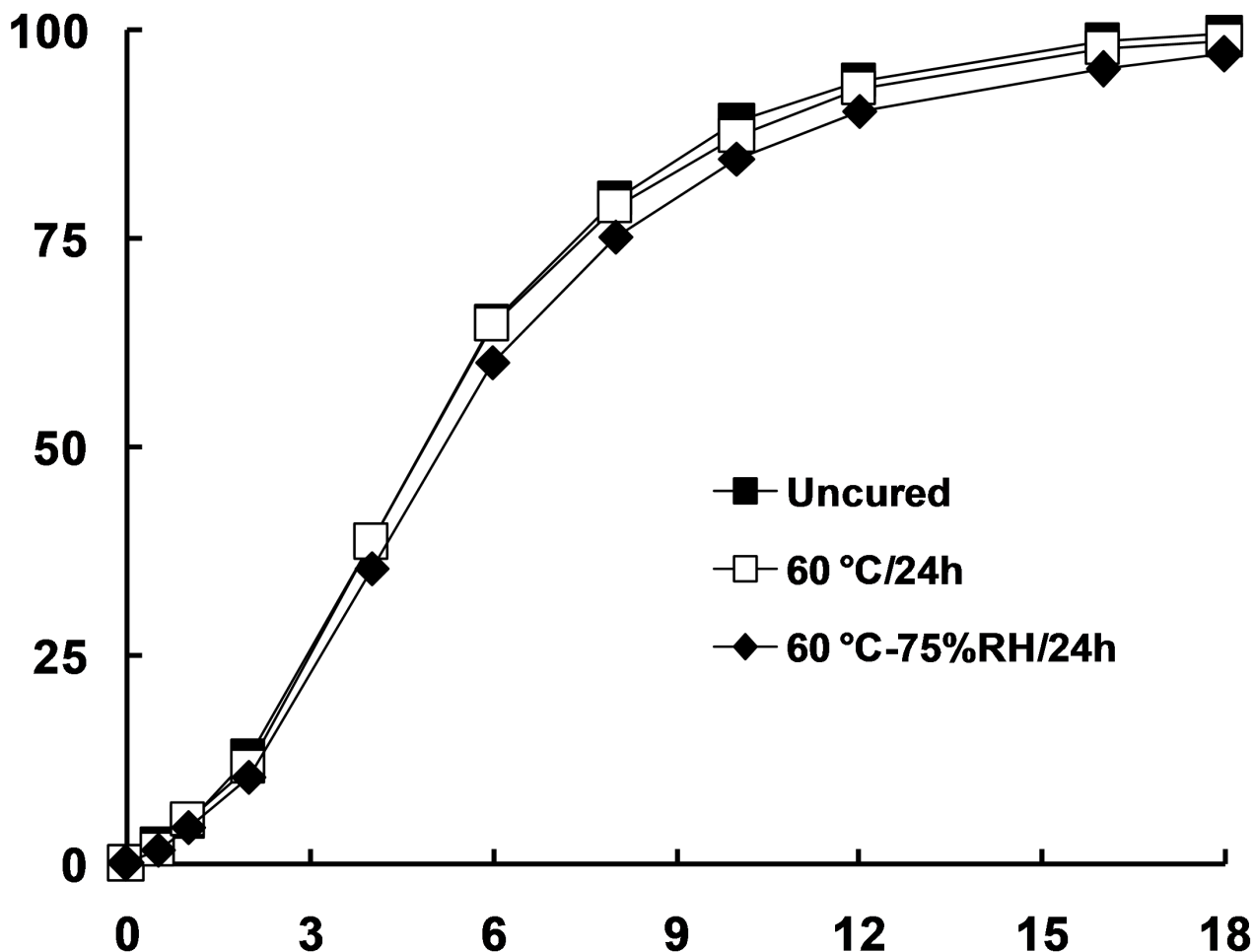
The video monitoring during dissolution of the uncured and cured pellets revealed the similar swelling behavior with uniform increase in size without local swelling (Figure 11A-D).

The adhesive force of the coating to the drug-layered-cores was not affected upon curing at elevated temperature and humidity (60 °C-75%RH) (Figure 12).

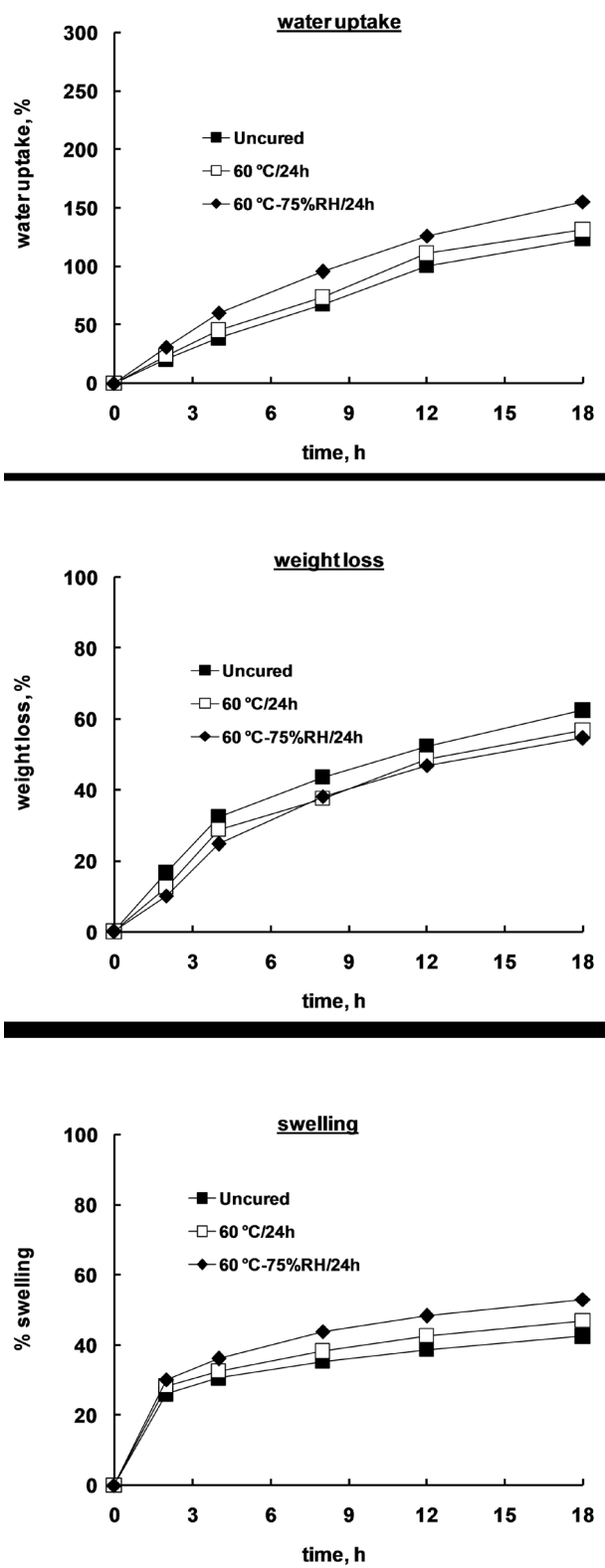
The pellets coated with Eudragit® NE 30D: Aquacoat® ECD (25:75) with no curing effect remained

stable at 40 °C and 40 °C-75%RH up to 3 months (Figure 13A-B).

The results allow us to infer that blend of Eudragit® NE 30D: Aquacoat® ECD not only compensated the poor film formation, but also prevented the decrease in adhesive force observed to Eudragit® NE 30D coatings. Probably, the addition of Eudragit® NE 30D, with low Tg (-8 °C), plasticized the Aquacoat® ECD to some extent, reducing its Tg from 135 °C to 123 °C (Table I) (Zheng, McGinity, 2003).

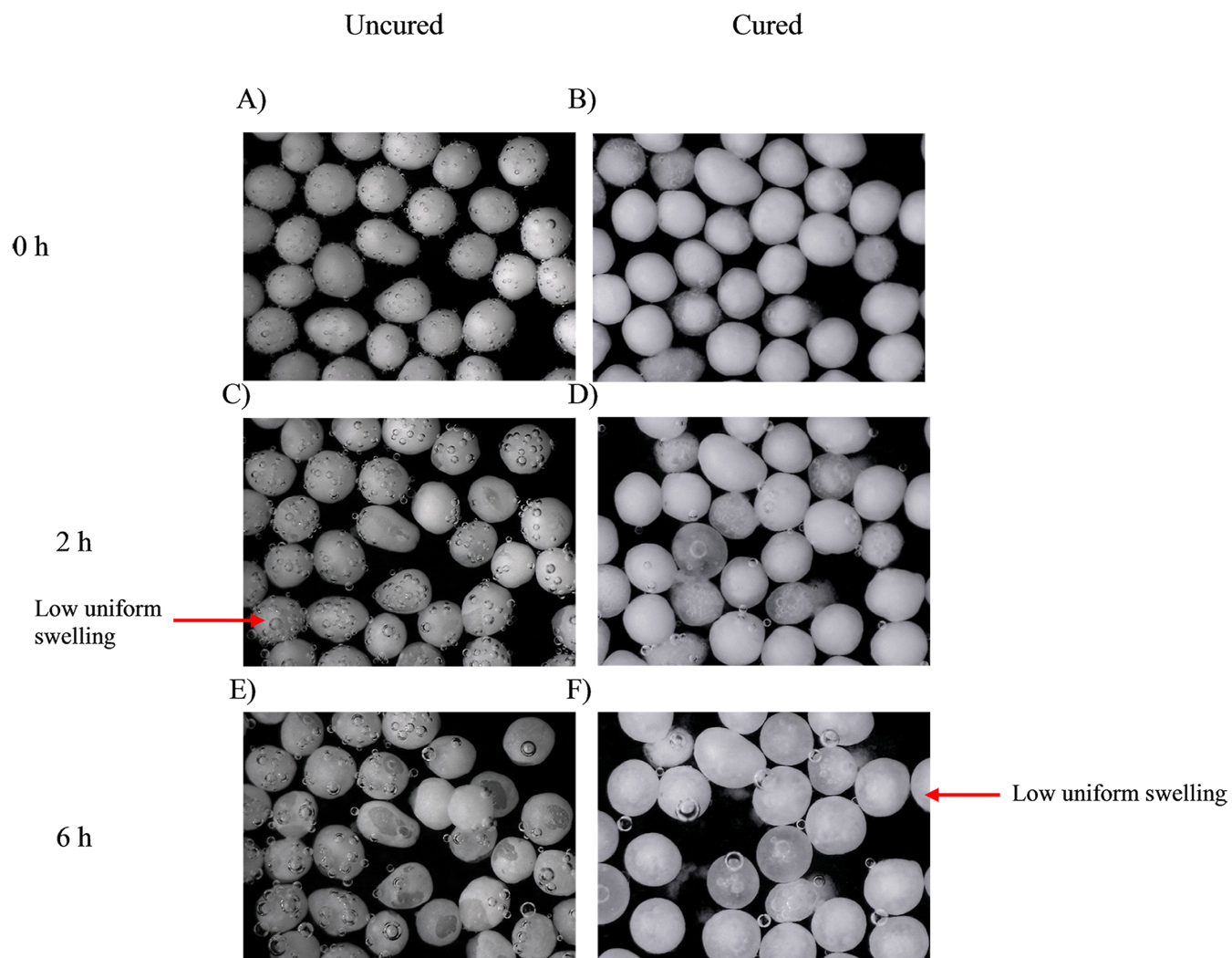


**FIGURE 9** - Effect of curing on drug release from pellets based on sugar cores loaded with 10% propranolol HCl and coated with a polymer blend of Eudragit® NE 30D: Aquacoat® ECD (25:75) using 35% talc, coating level 20%.

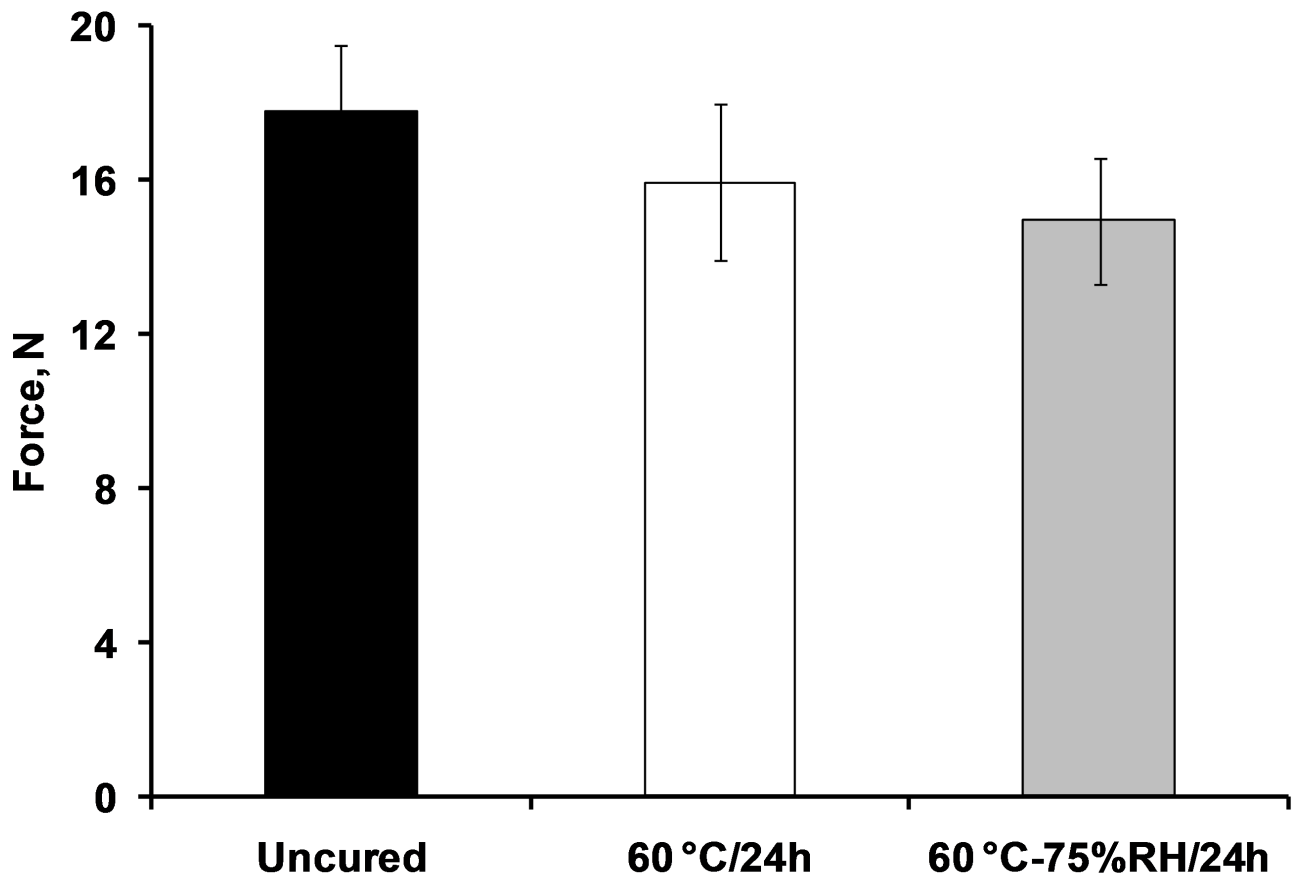


**FIGURE 10** - Water uptake-weight loss and swelling of uncured and cured pellets as a function of time in 0.01 N HCl based on sugar cores loaded with 10% propranolol HCl and coated with a polymer blend of Eudragit® NE 30D: Aquacoat® ECD (25:75) using 35% talc, coating level 20%.

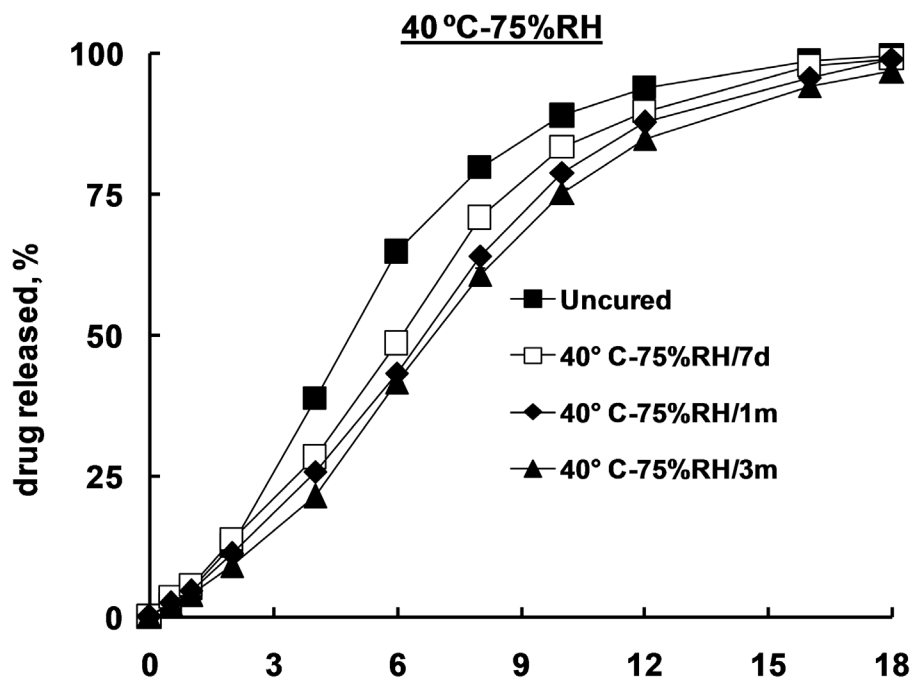
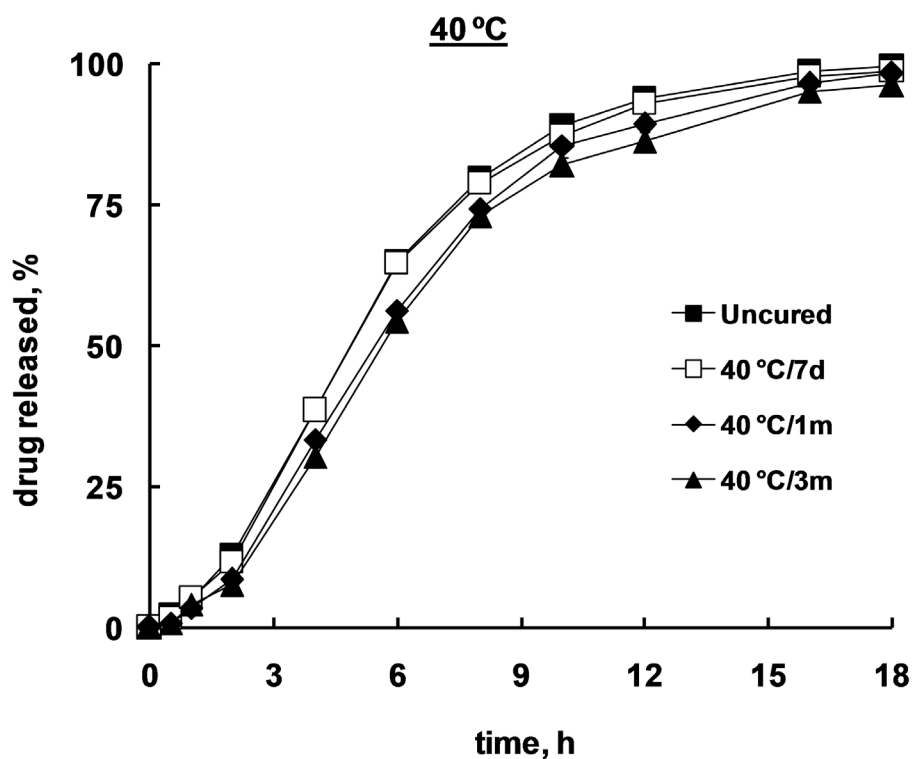




**FIGURE 11** - Macroscopic pictures of uncured and cured (60 °C/75% RH/24 h) pellets based on sugar cores loaded with 10% propranolol HCl coated with Eudragit® NE 30D: Aquacoat® ECD (25:75) using 35% talc as a function of time in 0.01 N HCl.



**FIGURE 12** - Effect of curing on adhesive force of Eudragit® NE 30D: Aquacoat® ECD (25:75) polymeric coatings to the drug-layered-cores using model tablets (drug layered and polymer coated like pellets), coating level 20%.



**FIGURE 13** - Effect of accelerated storage conditions on the stability of propranolol HCl release from pellets based on sugar cores with 10% drug loading and coated with a polymer blend of Eudragit® NE 30D: Aquacoat® ECD (25:75) using 35% talc, coating level 20%.

**TABLE I** - Glass transition temperature ( $T_g$ ) of Eudragit® NE 30D, Aquacoat® ECD and blend of Eudragit® NE 30D: Aquacoat® ECD (75:25)

Polymer	Glass Transition Temperature ( $T_g$ ), °C
Eudragit® NE 30D	8
Aquacoat® ECD	135
Eudragit® NE 30D: Aquacoat® ECD (25:75)	125

## CONCLUSION

A strong curing effect (decrease in drug release) was observed with pellets coated with individual Eudragit® NE 30D and Aquacoat® ECD, depicting entirely different curing mechanisms. According to the found curing mechanisms; Aquacoat® ECD coated pellets showed curing effect probably due to further gradual coalescence of polymeric particles upon storage at elevated temperature and humidity which resulted into better film formation, ultimately, decreasing the drug release. In contrast, the curing effect of Eudragit® NE 30D coated pellets was caused by decrease in adhesive force of coatings to the drug-layered-cores after treatment at elevated temperature and humidity providing a completely different swelling behavior of uncured (localized swelling) and cured (uniform swelling) pellets. The curing effect was eliminated using their blends in appropriate ratio, compensated the main irregularities associated with these individual polymers (Aquacoat® ECD – further gradual coalescence and Eudragit® NE 30D – decreased adhesive force of coating).

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