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ORIGINAL RESEARCH

Lung perfusion and emphysema distribution affect the outcome of endobronchial valve therapy

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Abstract: The exclusion of collateral ventilation (CV) and other factors affect the clinical success of endoscopic lung volume reduction (ELVR). However, despite its benefits, the outcome of ELVR remains difficult to predict. We investigated whether clinical success could be predicted by emphysema distribution assessed by computed tomography scan and baseline perfusion assessed by perfusion scintigraphy. Data from 57 patients with no CV in the target lobe (TL) were retrospectively analyzed after ELVR with valves. Pulmonary function tests (PFT), St George's Respiratory Questionnaire (SGRQ), and 6-minute walk tests (6MWT) were performed on patients at baseline. The sample was grouped into high and low levels at the median of TL perfusion, ipsilateral nontarget lobe (INL) perfusion, and heterogeneity index (HI). These groups were analyzed for association with changes in outcome parameters from baseline to 3 months follow-up. Compared to baseline, patients showed significant improvements in PFT, SGRQ, and 6MWT (all $P \le 0.001$). TL perfusion was not associated with changes in the outcome. High INL perfusion was significantly associated with increases in 6MWT (P=0.014), and high HI was associated with increases in forced expiratory volume in 1 second (FEV,), (P=0.012). Likewise, there were significant correlations for INL perfusion and improvement of 6MWT (r=0.35, P=0.03) and for HI and improvement in FEV, (r=0.45, P=0.001). This study reveals new attributes that associate with positive outcomes for patient selection prior to ELVR. Patients with high perfusions in INL demonstrated greater improvements in 6MWT, while patients with high HI were more likely to respond in FEV₁.

Keywords: endoscopic lung volume reduction, COPD, valves, lung perfusion, emphysema distribution

Introduction

Endoscopic lung volume reduction (ELVR) with valves has been shown to improve lung function, exercise capacity, and quality of life in selected patients with severe lung emphysema.^{1–5} However, a large spectrum of clinical treatment responses has been observed, emphasizing the importance of patient selection prior to treatment.¹ Although the selection criteria for ELVR have recently improved, it remains a challenge for clinicians to identify those patients with the highest benefit–risk ratio.

The development of target lobe (TL) atelectasis is an important surrogate marker for clinical response.^{6,7} A TL volume reduction of >350 mL has been defined in several studies as indicative of significant lobe volume reduction associated with clinical benefits.⁸ Recent post hoc analyses of large studies have identified complete lobular occlusion by valves and the exclusion of interlobar collateral ventilation (CV) as important predictive factors.^{9–12} CV is defined as the ventilation between lobes that bypasses the normal airways.¹³ The importance of CV to the outcome of ELVR was recently demonstrated by a prospective sham-controlled randomized trial.² It has become clinical routine to assess

International Journal of COPD 2016:11 1245-1259

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interlobar CV by the analysis of fissure integrity from computed tomography (CT) scans or by endobronchial in vivo measurement using the Chartis system. Both techniques have shown comparable accuracies.^{14–16}

CT scans and ventilation/perfusion scintigraphy are routinely performed to better characterize COPD lungs prior to ELVR.^{1,16–18} While emphysema heterogeneity is widely used as a selection criterion for ELVR treatment, its role is currently under discussion: in the original North American VENT study cohort, heterogeneous emphysema distribution predicted improvement in the 6-minute walk test (6MWT) and in the forced expiratory volume in 1 second (FEV₁).¹ In contrast, the European VENT cohort and two recent studies did not find a difference in outcome parameters for homogenous or heterogeneous emphysema distribution.^{6,9,16}

Low perfusion of the upper lobes, as assessed by ventilation/perfusion scans, was shown to associate with less mortality¹⁹ following lung volume reduction surgery, the surgical equivalent of ELVR. When lung perfusion was taken into consideration for ELVR, a recent study suggested that patients with low perfusion of the TL demonstrated more improvement in exercise capacity after ELVR than patients with high perfusion in the TL.¹⁷

In the context that CT and ventilation/perfusion scans are important tools for assessing COPD patients prior to ELVR, we investigated whether emphysema distribution and baseline perfusion of lung lobes help to predict the clinical outcome of ELVR with valves.

Materials and methods

Patients

We retrospectively analyzed 57 patients treated with ELVR between September 2011 and July 2014 at the Charité Hospital in Berlin, Germany. The study design was approved by the ethics committee of the Charité Universitätsmedizin Berlin (EA1/064/12). All patients provided written informed consent. Inclusion criteria for ELVR were age over 40 years, diagnosis of COPD with FEV, below 45% predicted, and nonsmoker status for at least 3 months proven by HbCO below 2.0%. No ELVR was performed on patients with signs of an infection, myocardial infarction in the past 6 months, and severe comorbidities (malignant disease, severe bronchiectasis, asthma, pulmonary hypertension, and lung fibrosis). For the retrospective analysis, we further excluded patients with $\alpha 1$ antitrypsin deficiency, CV in the TL as detected by the Chartis system, and implantation of valves in the middle lobe, and missing follow-up examination.

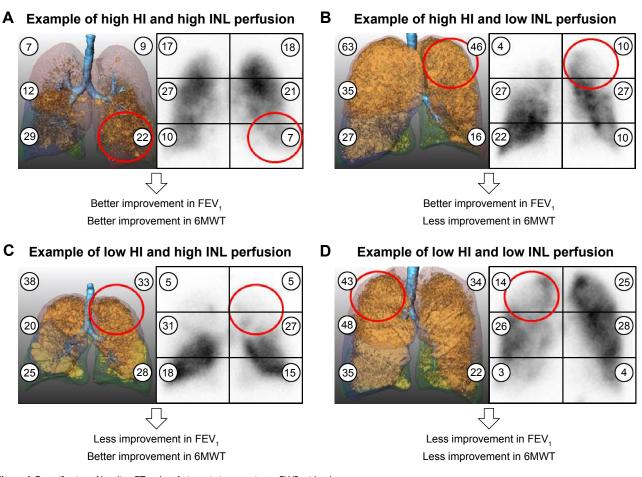
Prior to ELVR, all patients underwent pulmonary function tests (PFT) for FEV₁, vital capacity (VC), residual volume

(RV), diffusing capacity of the lung for carbon monoxide (corrected for lung volume) (KCO), as well as 6MWT and St George's Respiratory Questionnaire (SGRQ), which ranges from 0 to 100, with higher scores associating with lower quality of life. Low-dose CT under deep inspiration and ventilation/perfusion scintigraphy was performed on patients to assess emphysema distribution and lobe perfusion in the lung. Patients without contraindications for ELVR from these evaluations further received a Chartis assessment (Pulmonx, Redwood City, CA, USA) to exclude possible CV. A team of pneumologists and radiologists defined the primary and alternative TL according to the most emphysematous lobes in the CT scan. If multiple lobes showed a high degree of emphysema, lobes with less perfusion in the scintigraphy were preferred. The perfusion of the ipsilateral adjacent lobe was not considered for TL selection. Finally, the primary or alternative TL was chosen for treatment if no CV was detected in the Chartis assessment. The patients were hospitalized for the ELVR valve treatment. Endobronchial one-way silicone valves (Zephyr, Pulmonx) were implanted in the bronchus via a flexible delivery catheter, and the TL was completely occluded with valves. Follow-up assessment of the patients 3 months later included another CT scan, PFT, 6MWT, and SGRQ. The data were compared to baseline values.

Because left lungs were found to be more frequently negative for CV, ELVR was more often performed in the left lung: right upper lobe (RUL; n=7), right lower lobe (RLL; n=4), left upper lobe (LUL; n=13), and left lower lobe (LLL; n=33).

Perfusion scintigraphy

Lung perfusion was assessed using a combined single-photon emission computed tomography (SPECT) and CT system. Technical details of the procedure are available in the supplementary material. Only the posterior-to-anterior planar views were analyzed due to the lack of software-based quantification tools for SPECT. Each lung perfusion scintigram was split craniocaudally into three regions to quantify the distribution of the tracer in the lungs. The perfusion was calculated as the percentage of tracer activity in the upper, middle, and lower regions of the right and left lung. The upper region perfusion was used as a surrogate for upper lobe perfusion, and the lower region perfusion was used as a surrogate for lower lobe perfusion, as recently described.¹⁷ The perfusion of the middle region was not considered for further analyses. Figure 1 shows examples of different perfusion scintigrams. Three patients had no ventilation and perfusion scintigraphies and were excluded from the analyses of TL and ipsilateral nontarget lobe (INL) perfusion.



 $\label{eq:Figure I} \mbox{ Quantification of baseline CT and perfusion scintigrams prior to ELVR with valves}.$

Notes: CT scans on inspiration were assessed by MeVisPULMO^{3D} for segmentation of emphysema clusters in the lung. The brown colored areas show pixels of <-950Hounsfield units, suggestive of emphysema. The numbers in the CT indicate the percentage of emphysema in each lung lobe relative to the total number of voxels in the respective lobe. The HI is defined as the difference in emphysema score between TL and INL. A high HI indicates a more heterogeneous emphysema. The numbers in the perfusion scintigrams indicate the tracer activity in the respective region as percentage of both lungs, calculated for the geometric mean. The patients were grouped into high and low levels of the medians of HI (12.2%) and INL perfusion (14.7%) among all patients. The red circle marks the TL for ELVR. Views are from anterior to posterior. (A) Example of a patient with high HI (13%) and high INL perfusion (18%). (B) Example of a patient with high HI (30%) and low INL perfusion (10%). (C) Example of a patient with low HI (5%) and high INL perfusion (15%). (D) Example of a patient with low HI (8%) and low INL perfusion (3%).

Abbreviations: CT, computed tomograms; ELVR, endoscopic lung volume reduction; FEV₁, forced expiratory volume in I second; 6MWT, 6-minute walk test; HI, heterogeneity index; TL, target lobe; INL, ipsilateral nontarget lobe.

Low-dose CT scans

Patients underwent a CT scan for TL selection and emphysema evaluation at baseline and 3 months after endoscopic valve implantation as follow-up. All patients were examined using the same CT scanner (General Electric LightSpeed Ultra 8, General Electric Inc, Milwaukee, WI, USA) and the same scanning protocol (continuous helical scan of the whole lung in deep inspiratory breath hold, no intravenous contrast agent, primary slice thickness 1.25 mm, 100 kV voltage, and 100 mA current). Reconstruction of the raw CT data was performed using a "standard" (soft tissue) kernel. Quantitative analysis of lung parenchyma from CT data was performed semiautomatically using the MeVisPULMO3D software (v3.42, Fraunhofer MeVis, Bremen, Germany). The software was able to evaluate the distribution of emphysema by calculating the pixel index, defined as the ratio of lung voxels with a density <-950 Hounsfield units to the total number of voxels in the lung per lobe, which also is the emphysema score per lobe. The heterogeneity index (HI) was defined as the difference in emphysema score between TL and ipsilateral nontarget upper or lower lobe, as previously reported.^{1,9,20} The middle lobe was not considered for further analyses. Figure 1 shows examples of different emphysema distributions. TL volume reduction was calculated as the difference between TL volume at baseline and TL volume at follow-up. Three patients had no baseline CT data and were excluded from the heterogeneity analysis.

Statistics

First, patients were grouped into high and low levels at 1) the median of TL perfusion (Table S1), 2) the median of INL perfusion (Table 1), and 3) the median of HI (Table 2).

Table I	Patient baseline	characteristics and	clinical	outcome with	respect to	baseline INL	perfusion
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Parameters	Below median INL perfusion (<14.7%)	Above median INL perfusion (>14.7%)	P-value
n	27	27	
Baseline INL perfusion	. ±3.2	17.9±3.2	0.001
Sex, n, (male/female)	19/8	12/15	ns
Age (yr)	67.8±5.7	68.5±5.5	ns
BMI (kg/m ²)	26.9±4.4	23.7±4.9	0.023
Smoking history (pack-yr)	49.7±18.2	46.5±23.8	ns
HI <12.2%	12	13	ns
HI ≥12.2%	13	13	
Treatment site			0.002
RUL	3	4	
RLL	I	3	
LUL	12	I	
LLL	II	19	
Baseline FEV ₁ (% pred)	27.4±7.4	25.9±6.4	ns
Baseline VC (% pred)	67.2±13.7	61.7±12.4	ns
Baseline RV (% pred)	212±44	222±31	ns
Baseline TLC (% pred)	121±16	123±11	ns
Baseline KCO (% pred)	32.3±18.1	39.0±21.3	ns
Baseline 6MWT (m)	240±81	212±96	ns
Baseline SGRQ (points)	64.0±11.7	65.8±14.1	ns
ΔFEV_{\downarrow} (%)	24.9±26.1	22.2±23.8	ns
ΔVC (%)	17.4±21.9	12.0±21.1	ns
∆RV (%)	-6.7±16.9	-8.8±18.6	ns
ΔTLC (%)	-0.1±8.0	-3.I±II.7	ns
∆Ксо (%)	38.9±57.1	23.6±55.9	ns
∆6MWT (m)	8.0±45.3	58.8±69.6	0.014
Δ SGRQ (points)	-7.2±13.9	-11.8±13.7	ns

Notes: Data are presented as mean \pm standard deviation. *P*-values were calculated for categorical variables using the chi-square test and Fisher's exact test and for continuous variables using the Mann–Whitney *U*-test.

Abbreviations: INL, ipsilateral nontarget lobe; ns, not significant; BMI, body mass index; HI, heterogeneity index; RUL, right upper lobe; RLL, right lower lobe; LUL, left upper lobe; LLL, left lower lobe; FEV,, forced expiratory volume in 1 second; VC, vital capacity; RV, residual volume; TLC, total lung capacity; KCO, diffusing capacity of the lung for carbon monoxide (corrected for lung volume); 6MWT, 6-minute walk test; SGRQ, St George's Respiratory Questionnaire; Δ , change from baseline to follow-up.

Between these groups, the changes in the outcome parameters (PFT, SGRQ, and 6MWT) were compared. Next, correlations were calculated between TL perfusion, INL perfusion, HI, and the changes in the outcome parameters. The chi-square test and the Fisher's exact test were used for the statistical analysis of categorical variables. The Mann–Whitney *U*-test was used for continuous variables. The Wilcoxon test was used for paired samples, eg, changes in the outcome parameters from baseline to follow-up. Correlations were assessed by Pearson's correlation coefficient and Student's *t*-test. All tests were two-tailed. SPSS Statistics Version 22 (IBM Corporation, Armonk, NY, USA) was used for all analyses. The data are presented as mean \pm standard deviation. A *P*-value <0.05 was considered statistically significant.

Results

Fifty-seven patients, assessed to be negative for CV by Chartis, were treated with endobronchial valves. Compared to baseline,

all patients demonstrated at follow-up a mean volume reduction in the TL of 1,184±577 mL, an improvement in FEV₁ of 23.8%±24.9%, RV of $-8.0\%\pm17.3\%$, VC of 15.9%±23.2%, SGRQ of -10.1 ± 14.0 points, and 6MWT of 34.6±62.3 m (all $P \le 0.001$, Figure 2). Further details are listed in Table S2.

The baseline characteristics and outcome data for TL perfusion, INL perfusion, and HI groups are listed in Tables 1, 2 and S1. The TL perfusion ranged from 1.8% to 19.9% with a median of 8.11% (Table S1), the INL perfusion ranged from 3.4% to 25.7% with a median of 14.7% (Table 1), and HI ranged from 0.6% to 32.8% with a median of 12.2% (Table 2). The median perfusion was lowest in LLL (8.8%), compared to LUL (14.7%), RLL (13.4%), and RUL (13.4%). With respect to HI, 27 patients were categorized in the homogeneous emphysema group and 27 patients were in the heterogeneous emphysema group (cutoff 12.2%).

There were no significant correlations between TL perfusion and HI as well as INL perfusion and HI (Figure 3).

Parameters	Homogeneous emphysema (<12.2% HI)	Heterogeneous emphysema (≥12.2% HI)	P-value
n	27	27	
Baseline HI	6.4±3.3	21.2±6.5	0.001
Sex, n, (male/female)	15/12	6/	ns
Age (yr)	66.6±5.3	69.0±5.9	ns
BMI (kg/m ²)	25.5±4.5	24.3±5.4	ns
Smoking history (pack-yr)	48.7±25.9	47.2±15.3	ns
Treatment site			ns
RUL	6	I	
RLL	3	I	
LUL	5	7	
LLL	13	18	
Baseline FEV ₁ (% pred)	26.6±7.3	25.7±6.9	ns
Baseline VC (% pred)	64.4±13.7	64.0±13.8	ns
Baseline RV (% pred)	215±31	215±36	ns
Baseline TLC (% pred)	121±13	121±11	ns
Baseline KCO (% pred)	31.4±16.7	37.9±22.4	ns
Baseline 6MWT (m)	232±77	215±96	ns
Baseline SGRQ (points)	64.I±I4.4	66.8±11.7	ns
∆FEV, (%)	14.9±19.9	32.7±27.3	0.012
ΔVC (%)	14.9±23.3	16.7±23.8	ns
ΔRV (%)	-7.8±14.9	-7.8±20.0	ns
ΔTLC (%)	-1.7±9.5	-1.7±10.7	ns
∆Ксо (%)	31.3±52.9	29.1±60.1	ns
∆6MWT (m)	32.8±73.9	38.2±50.8	ns
∆SGRQ (points)	-9.8±14.6	-10.1±14.3	ns

Table 2 Patient baseline characteristics and clinical outcome with respect to baseline HI
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Notes: Data are presented as mean \pm standard deviation. *P*-values were calculated for categorical variables using the chi-square test and Fisher's exact test and for continuous variables using the Mann–Whitney *U*-test.

Abbreviations: HI, heterogeneity index; ns, not significant; BMI, body mass index; RUL, right upper lobe; RLL, right lower lobe; LLL, left upper lobe; LLL, left lower lobe; FEV₁, forced expiratory volume in I second; VC, vital capacity; RV, residual volume; TLC, total lung capacity; KCO, diffusing capacity of the lung for carbon monoxide (corrected for lung volume); 6MVVT, 6-minute walk test; SGRQ, St George's Respiratory Questionnaire; Δ , change from baseline to follow-up.

Likewise, the distribution of patients into the four group combinations of low or high TL perfusion and low or high HI was not significantly different (P=0.58, Table S3). The same was observed for the groups of low and high INL perfusion and low or high HI (P=1.0, Table S3).

Comparing TL perfusion, INL perfusion, and HI to outcome parameters, low vs high TL perfusion was not associated with any outcome indices (Table S1). In contrast, patients with INL perfusion >14.7% demonstrated a higher increase in 6MWT than patients with INL perfusion below 14.7% (P=0.014), while the other outcome parameters were similar for both groups (Table 1). Likewise, patients with HI >12.2% had a higher improvement in FEV₁ than patients with HI <12.2% (P=0.012), while the other outcome parameters were similar for both groups (Table 2).

To confirm these results, TL perfusion, INL perfusion, and HI were tested for correlation with the outcome parameters. Likewise, no significant correlation was identified between TL perfusion and any change in clinical outcome (Figure S1). Again, INL perfusion was significantly correlated only with changes in the 6MWT between baseline and follow-up (r=0.35, P=0.03; Figure 4A), and not with changes in TL volume (r=-0.05, P=not significant [ns]), FEV, (r=0.01, P=ns), RV (r=-0.10, P=ns), VC (r=0.07, P=ns), KCO (r=-0.08, P=ns), and SGRQ (r=-0.11, P=ns; Figure S2). Similarly, HI demonstrated a significant correlation only with changes in FEV, (r=0.45, P=0.001; Figure 4B), but not with changes in TL volume (r=-0.09, P=ns), RV (r=-0.12, P=ns), VC (r=0.14, P=ns), SGRQ (r=-0.15, P=ns), KCO (r=-0.05, P=ns), and 6MWT (r=0.05, P=ns; Figure S3). Interestingly, improvement of 6MWT of 50.8 m among patients with high INH perfusion compared to low INL perfusion was independent of the HI (Figure 5A and C), and, likewise, improvement of FEV, of 17.8% among patients with high HI compared to low HI was not associated with INL perfusion (Figure 5B and D).

Discussion

In this study, we found a significant correlation between high INL perfusion and larger improvement in the 6MWT and

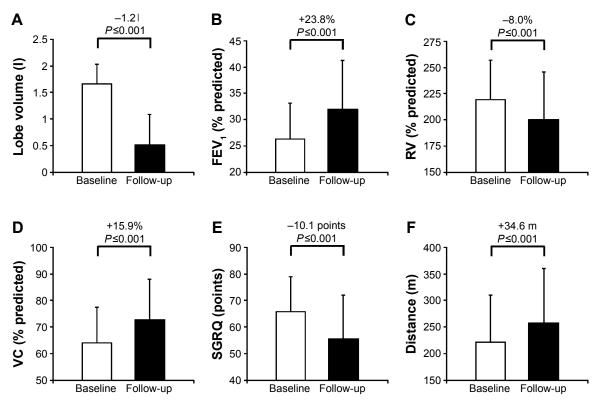


Figure 2 Clinical outcomes of patients after ELVR with valves.

Notes: The parameters were assessed prior to and 3 months after treatment. *P*-values were calculated using the Wilcoxon test. (**A**) TLV. TLV was quantified from computed tomograms before and after ELVR using the MeVisPULMO^{3D} software. (**B**) FEV₁. (**C**) RV. (**D**) VC. (**E**) SGRQ. (**F**) 6MWVT. Data are presented as mean and standard deviation. Numbers indicate relative change.

Abbreviations: ELVR, endoscopic lung volume reduction; TLV, target lobe volume; FEV, forced expiratory volume in 1 second; RV, residual volume; VC, vital capacity; SGRQ, St George's Respiratory Questionnaire; 6MWT, 6-minute walk test.

between a high HI and larger improvement in FEV_1 . Analyzing subgroups, patients with high INL perfusion (cutoff 14.7%) benefited from a greater improvement of 50.8 m in the 6MWT compared to those with low INL perfusion, while patients with a heterogeneous emphysema distribution

(cutoff 12.2% HI) showed a higher increase in FEV₁ of 17.8% compared to those with low HI.

Important factors were recently characterized to predict the clinical success of ELVR. Several studies suggest that ELVR is an effective treatment option if complete lobar

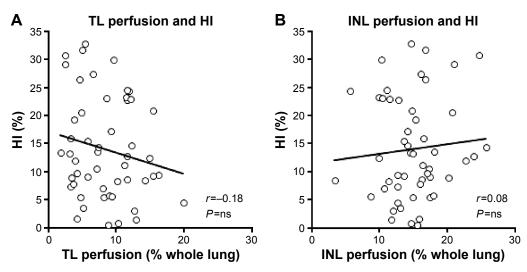


Figure 3 Correlation between lung perfusion and HI.

Notes: The HI is defined as the difference in emphysema score between TL and INL. *P*-values were calculated using the Student's *t*-test. (A) Correlation between HI and perfusion of the TL. (B) Correlation between HI and perfusion of the INL.

Abbreviations: HI, heterogeneity index; TL, target lobe; INL, ipsilateral nontarget lobe; r, Pearson's correlation coefficient; ns, not significant.

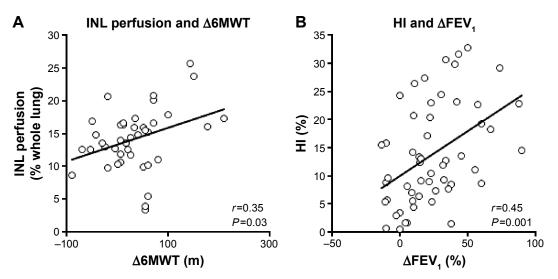


Figure 4 Correlations between perfusion of the INL, HI and outcome parameters.

Notes: *P*-values were calculated using the Student's t-test. (A) Correlation between INL perfusion and change in $\Delta 6$ MWT after ELVR. (B) Correlation between HI and ΔFEV , after ELVR.

Abbreviations: INL, ipsilateral nontarget lobe; HI, heterogeneity index; 6MVVT, 6-minute walk test; ELVR, endoscopic lung volume reduction; FEV₁, forced expiratory volume in I second; *r*, Pearson's correlation coefficient; Δ , change from baseline to follow-up.

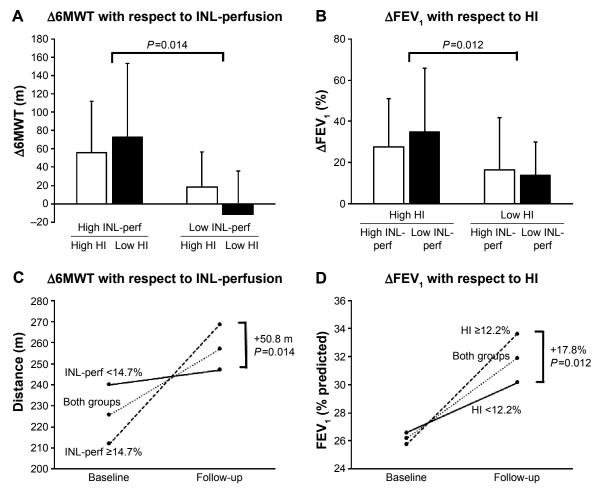


Figure 5 Clinical outcome according to baseline percentage perfusion of the INL and the HI.

Notes: P-values were calculated using the Mann–Whitney U-test. (**A** and **C**) Change in 6MWT relative to INL perfusion. High INL perfusion includes all patients with INL perfusion >14.7%. (**B** and **D**) Change in FEV, relative to HI. High HI includes all patients with a difference in emphysema scores between TL and INL of >12.2%. Low HI includes all patients with a difference in emphysema scores between TL and INL of <12.2%. Abbreviations: INL, ipsilateral nontarget lobe; HI, heterogeneity index; 6MWT, six-minute walk test; FEV, forced expiratory volume in I second; perf, perfusion; TL, target lobe; INL, ipsilateral nontarget lobe; Δ , change from baseline to follow-up.

occlusion with valves is achieved.^{2,8–10} In line, other studies have shown valve treatment to be less efficient, if valves were placed in both lungs without the goal of lobar occlusion.^{11,12} A post hoc analysis of the US- and Euro-VENT studies identified a subset of patients who had no CV and who achieved higher lung volume reduction and greater clinical response.^{1,9} The importance of the absence of CV to the outcome was recently confirmed by the BeLieVeR-HIFi study in a randomized, sham-controlled study design.² Subsequently, it has become routine practice to assess interlobar CV by analysis of fissure integrity on high-resolution CT scan or by real-time endobronchial in vivo measurement with the Chartis system.^{3,4,8,14}

This study suggests that INL lung perfusion significantly predicts the improvement of the 6MWT after ELVR. Consequently, perfusion scintigraphy seems to be an important criterion for baseline evaluation of patients prior to ELVR. Among COPD patients, we observed a large variability of TL and INL perfusions ranging from very high to extreme low, which supports the concept of COPD heterogeneity.^{21,22} In this context, it is important to note that the perfusion of TL or INL is calculated as a percentage of the perfusion of the total lung. Therefore, a seemingly homogeneously perfused COPD lung might be severely impaired due to homogeneous parenchymal destructions of the lung. Similar to other authors, we found an association between perfusion and emphysema score (Figure S4).²³ Interestingly, however, we also identified severe hypoperfused regions irrespective of the emphysematic changes, suggesting other pulmonary vascular abnormalities such as local vascular inflammation with remodeling to be relevant to these COPD lungs.24,25

It remains unclear how perfusion affects improvements in the 6MWT after ELVR. The 6MWT is a predictor of mortality in patients with severe emphysema and has been established in the evaluation of COPD patients.²⁶⁻²⁸ It reflects the exercise capacity of patients based on the pulmonary, cardiovascular, and muscular systems. Chung et al²⁹ first examined perfusion in patients treated with ELVR and reported that perfusion decreased in the treated lung, while it increased in the contralateral lung. This was confirmed by other studies, which specified that after the treated lobe was reduced in volume, the perfusion and volume was redirected to the INL and to the contralateral lung.^{18,30,31} This interesting finding suggests that both the INL and contralateral lung take over functionality after development of an atelectasis of the TL, which explains the importance of the INL.32

However, while we did not find an effect of TL perfusion on the 6MWT, a recent study by Argula et al¹⁷ reports a better 6MWT performance in patients with low TL perfusion. This may be due to the fact that we mostly treated the lower lobes of patients, which were already associated with less perfusion, while Argula et al¹⁷ mostly treated the upper lobes of patients. Moreover, Argula et al's¹⁷ data also consisted of a slightly higher proportion of patients with heterogeneous lung emphysema in comparison to our study group. Nevertheless, high INL perfusion seems to be an indicator of a relatively healthier functional lobe, while low TL perfusion probably indicates a more damaged lobe. We hypothesize that the findings of improved 6MWT in low TL perfusion and high INL perfusion may together represent an optimal setting for ELVR: a more functional INL with high perfusion and a more damaged TL with low perfusion.

Recent studies suggest that each lung lobe contributes differently to the pulmonary function; the lower lobes demonstrated a higher association to the FEV, than the upper lobes.^{33,34} In this study, mostly the LLL was treated, which might be another explanation why the changes in lung function were greater than in previous studies like the VENT study. However, because the lower lobes in general, and especially the LLL, were treated more often in this cohort, we cannot evaluate this effect due to the small number of patients in whom the upper lobes were treated. A small study by Eberhardt et al35 found no difference for the treatment of upper vs lower lobes with valves. Nevertheless, future studies with an equal distribution of the TL are needed to test for a different outcome of ELVR for each specific TL. Moreover, the recent interesting studies by Matsuo et al³³ and Kitano et al³⁴ used the normal lobar volume and the collapsibility index as CT-derived indices to analyze lobar physiology and function. These indices might be useful in the future to evaluate lung lobes prior to ELVR.

Another important finding of this study is the correlation of improvement in FEV_1 after ELVR to the baseline HI, suggesting a greater improvement of FEV_1 in patients with higher differences in the emphysema distribution between TL and the ipsilateral nontarget upper or lower lobe (middle lobes were not considered for HI calculations). There are several possible explanations for this observation: in lungs with heterogeneous emphysema, the TL consists of more bullae and cysts compared to the INL, while in homogeneous emphysema, both are more evenly distributed. Because these bullae and cysts are the main contributors to the hyperinflation, ELVR of the TL in a high heterogeneity lung may lead to a more significant reduction hyperinflation and consequently improve respiratory mechanics and air trapping. Moreover, compressed areas of the better-preserved adjacent lobes can reinflate to increase the surface of the lung to improve the gas exchange. This finding is in agreement with the North American VENT cohort reporting better clinical results in patients with heterogeneous compared to homogeneous emphysema.¹ However, some other studies have not observed these associations of emphysema distribution and outcome changes;^{6,9,16} therefore, further studies are urgently needed for clarification. Currently, a prospective randomized trial is studying the effect of ELVR in patients with homogeneous and heterogeneous lung emphysema and no CV.³⁶

A standardized definition of how to distinguish between heterogeneous and homogeneous lung emphysema is still lacking. In clinical routine and some other studies, heterogeneity is visually assessed on native CT scans,^{2,37,38} which is observer dependent and therefore highly variable. Software-based quantification tools allow investigators to quantify precisely the severity of emphysema in the lobes. Some studies converted the quantified emphysema score to a Likert scale to determine the HI.^{39,40} This study used the definition of the VENT study, which defined the HI as the difference in emphysema score between the target and the ipsilateral adjacent lobe.1 The median HI was 15% in the VENT study, which was used to split patients into low and high HI subgroups. The 15% median was suggested as an arbitrary cutoff marker for homogeneous and heterogeneous emphysema. Applying the same method, we split the patients into a low and high heterogeneity group at the median HI in this study. The median of 12.2% suggests a higher fraction of patients with homogeneous emphysema compared to the VENT. Nevertheless, there was a significant correlation between HI and FEV, improvement, indicating the predictive value of the HI regardless of a cutoff.

It is interesting to note that baseline HI was the main contributor of FEV_1 improvement, while INL perfusion was almost only associated with increases of 6MWT after ELVR. This suggess that morphologic changes of emphysematous damaged lobes are more likely to influence breathing mechanics, while INL perfusion shows higher correlations to exercise capacity. On the basis of the findings for INL perfusion and HI, we distinguished four COPD patient groups according to their baseline perfusion and HI in the TL: 1) patients with HI and high INL perfusion who were more likely to improve in FEV₁ and 6MWT; 2) patients with high HI and low INL perfusion who demonstrated better improvements in FEV₁, but less in 6MWT; 3) patients with low HI and high INL perfusion who showed less improvement in FEV₁ but higher 6MWT changes; and 4) patients with low HI and low INL who were less likely to respond in FEV_1 and 6MWT. Especially the last patient group might be a new subgroup to show limited response to ELVR even though this patient group fulfilled the other factors relevant to clinical success (significant hyperinflation in PFT, negative CV in TL, and complete lobar occlusion with valves).

Several possible limitations of this study should be considered. The division of planar perfusion scintigrams into thirds is only a rough estimation of lung perfusion and reduces the accuracy of the data. This limitation could be addressed in the future by software-based quantification tools for SPECT, which analyze the perfusion for each anatomical lung lobe. These tools showed impressive initial results, but are not yet widely used.^{41,42} Consequently, future studies should be performed using software-based quantification tools for SPECT to reassess the role of pulmonary perfusion for ELVR patient selection. However, because perfusion scintigraphy is already widely used prior to ELVR, the findings of this study are still highly relevant despite the limitations of planar perfusion imaging until SPECT is established in the clinical routine.

This is a retrospective analysis without blinding or patient randomization, and baseline characteristics are not evenly distributed, and so a selection bias cannot be excluded. CT scan and perfusion scintigraphy were also used for TL selection, which might bias the results. Therefore, prospective studies with well-matched and larger cohorts are urgently needed to confirm these results. Correlation analyses need careful interpretation due to the possible role of confounding variables, which might not have been considered. The only data that were evaluated were those in patients' files, as a consequence of the retrospective study design. We used the medians to discriminate between low and high INL perfusion and low and high HI; however, there might be better cutoff values for discriminating between the patient subgroups. To better understand the improvements in exercise capacity, other exercise tests, such as spiroergometry, are needed.

In summary, patient selection remains critical in ELVR because it bears the risk of severe complications.⁴³ Baseline HI and lobe perfusion may help to identify patients who benefit most from ELVR treatment. While patients with heterogeneous emphysema are more likely to profit from improved breathing mechanics, patients with high INL perfusion might benefit from improved exercise capacity. These predictors could be helpful in selecting both the patient and the TL for ELVR.

Acknowledgment

We thank Melanie Wegemund for her excellent assistance in data collection. This work is part of the doctoral thesis of Christian Thomsen.

Disclosure

Ralf-Harto Hubner has received lecture fees for educational activities and consulting fees from Pulmonx. The other authors have declared no conflict of interest in this work.

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Supplementary materials Online supplement

Technical details of perfusion scintigraphy

Ventilation and perfusion were assessed using a hybrid dual-head Siemens Symbia TruePoint T6 SPECT/CT system (Siemens Medical Solutions, Erlangen, Germany), which has a crystal thickness of 9.5 mm, and a 53.3 cm axial by 38.7 cm diameter single-photon emission computed tomography (SPECT) field of view. The scans were performed following a 1-day standard protocol: 128×128 acquisition matrix, zoom 1.0, pixel size 4.8 mm, and noncircular orbit (autocontour) with 30 projections over 180° (continuous acquisition). A low-energy high-resolution collimator was used with dual-energy windowing, and a lower scatter energy window (10% width) for scatter estimation. Thirty samples, each of 15 seconds duration, were used for both

the ventilation and the perfusion study. The total acquisition time was approximately 20 minutes. The seated patient inhaled about 60 MBq Tc-99m Technegas (Tema 10,000, Cyclomedica GmbH, Salzgitter, Germany) and the ventilation SPECT was performed. After the ventilation SPECT was performed, 100–120 MBq of 99 mTc-labeled human albumin macroaggregates (Mallinckrodt Medical BV, Petten, the Netherlands) were slowly injected intravenously while the patient took deep breaths. Perfusion tomography was then performed on the patient who was lying down. Only posterior-to-anterior planar views were used for further analyses due to the lack of software-based quantification tools for SPECT.

This study protocol was already described by the coauthors in another study using the same patients and procedure.¹

Table SI Patient baseline	characteristics and clinical	outcome with respect to	o baseline TL perfusion
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Parameters	Below median TL perfusion (<8.11%)	Above median TL perfusion (\geq 8.11%)	P-value
N	27	27	
Baseline TL perfusion	4.8±1.7	II.9±2.7	0.001
Sex, n, (male/female)	14/13	17/10	ns
Age (yr)	69.8±5.7	66.6±5.0	0.027
BMI (kg/m²)	25.1±5.1	25.5±4.8	ns
Smoking history (pack-yr)	42.3±15.9	53.6±24.0	ns
HI <12.2%	H	14	ns
HI ≥12.2%	14	12	
Treatment site			0.001
RUL	2	5	
RLL	0	4	
LUL	2	11	
LLL	23	7	
Baseline FEV ₁ (% pred)	27.4±6.5	25.8 ±7.3	ns
Baseline VC (% pred)	65.3±11.9	63.6±14.7	ns
Baseline RV (% pred)	217±40	217±36	ns
Baseline TLC (% pred)	123±17	120±11	ns
Baseline KCO (% pred)	43.4±23.0	28.9±13.9	0.042
Baseline 6MWT (m)	239±80	212±98	ns
Baseline SGRQ (points)	63.0±12.4	66.7±13.0	ns
ΔFEV_1 (%)	19.8±22.4	27.3±26.8	ns
ΔVC (%)	14.1±23.2	15.2±20.0	ns
ΔRV (%)	-9.8±17.9	-5.6±17.4	ns
∆TLC (%)	-3.2±11.2	-0.04±8.6	ns
∆Ксо (%)	17.4±52.6	42.1±57.8	ns
∆6MWT (m)	26.4±47.2	38.8±76.0	ns
Δ SGRQ (points)	-7.1±13.8	-11.9±13.8	ns

Notes: Data are presented as mean ± standard deviation. P-values were calculated for categorical variables using the chi-square test and Fisher's exact test, and for continuous variables using the Mann-Whitney U-test.

Abbreviations: TL perfusion, baseline percentage perfusion of TL; TL, target lobe; ns, not significant; BMI, body mass index; HI, heterogeneity index; RUL, right upper lobe; RLL, right lower lobe; LUL, left upper lobe; LLL, left lower lobe; FEV₁, forced expiratory volume in 1 second; VC, vital capacity; RV, residual volume; TLC, total lung capacity; KCO, diffusing capacity of the lung for carbon monoxide; SGRQ, St George's Respiratory Questionnaire; 6MVVT, 6-minute walk test distance; Δ , change from baseline to follow-up.

Table S2 Clinical outcome after ELVR

Parameters	Baseline	Follow-up	Absolute change	Relative change (%)	P-value
FEV, (% pred)	26.2±6.9	32.0±9.3	5.8±6.5	23.8±24.9	0.001
VC (% pred)	64.0±13.4	72.8±15.3	8.8±12.1	15.9±23.2	0.001
RV (% pred)	219±38	200±46	-18.7±37.1	-8.0±17.3	0.001
TLC (% pred)	123±14	120±17	-2.4±12.2	-1.8±9.9	0.129
KCO (% pred)	34.6±19.8	35.2±14.8	4.9±13.4	31.1±55.0	0.013
6MWT (m)	222±89	257±103	34.6±62.3	28.0±84.4	0.001
SGRQ (points)	65.7±13.3	55.4±16.6	-10.1±14.0	-15.4±20.4	0.001

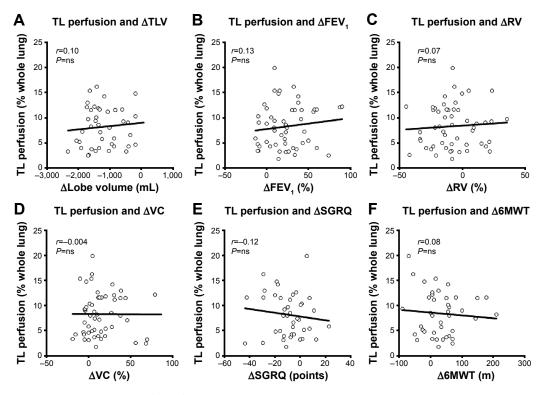
Notes: Data are presented as mean ± standard deviation. Numbers may not sum up to total due to rounding. *P*-values were calculated using the Wilcoxon test. **Abbreviations:** ELVR, endoscopic lung volume reduction; FEV₁, forced expiratory volume in 1 second; RV, residual volume; VC, vital capacity; TLC, total lung capacity; KCO, diffusing capacity of the lung for carbon monoxide; SGRQ, St George's Respiratory Questionnaire; 6MWT, 6-minute walk test distance.

Table S3 Patient groups with respect to perfusion and emphysema heterogeneity

	Low TL perfusion (<8.11%)	High TL perfusion (≥8.11%)	P-value
HI <12.2%	11	4	0.579
$HI \ge 12.2\%$	14	12	
	Low INL perfusion (<14.7%)	High INL perfusion (≥14.7%)	P-value
HI <12.2%	12	3	1.0
HI ≥12.2%	13	13	

Notes: Numbers indicate numbers of patients in each group. P-values were calculated using the chi-square test.

Abbreviations: TL, target lobe; HI, heterogeneity index; INL, ipsilateral nontarget lobe.





Notes: P-values were calculated using the Student's t-test. (A) Correlation between TL perfusion and Δ TLV. (B) Correlation between TL perfusion and Δ FV, (C) Correlation between TL perfusion and Δ RV. (D) Correlation between TL perfusion and Δ VC. (E) Correlation between TL perfusion and Δ SGRQ. (F) Correlation between TL perfusion and Δ SGRQ.

Abbreviations: TL, target lobe; Δ , change from baseline to follow-up; TLV, target lobe volume; *r*, Pearson's correlation coefficient; ns, not significant; FEV, forced expiratory volume in I second; RV, residual volume; SGRQ, St George's Respiratory Questionnaire; 6MWVT, 6-minute walk test distance; VC, vital capacity.

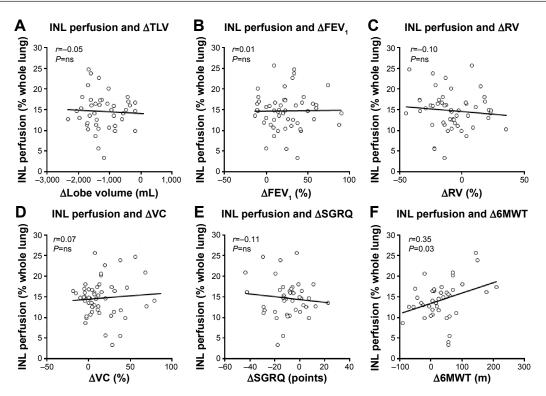


Figure S2 Correlations with baseline percentage perfusion of the INL.

Notes: P-values were calculated using the Student's t-test. (A) Correlation between INL perfusion and Δ TLV. (B) Correlation between INL perfusion and Δ FEV, (C) Correlation between INL perfusion and Δ RV. (D) Correlation between INL perfusion and Δ VC. (E) Correlation between INL perfusion and Δ SGRQ. (F) Correlation between INL perfusion and Δ SGRQ.

Abbreviations: INL, ipsilateral nontarget lobe; Δ , change from baseline to follow-up; TLV, target lobe volume; *r*, Pearson's correlation coefficient; ns, not significant; FEV₁, forced expiratory volume in I second; RV, residual volume; SGRQ, St George's Respiratory Questionnaire; 6MWT, 6-minute walk test distance; VC, vital capacity.

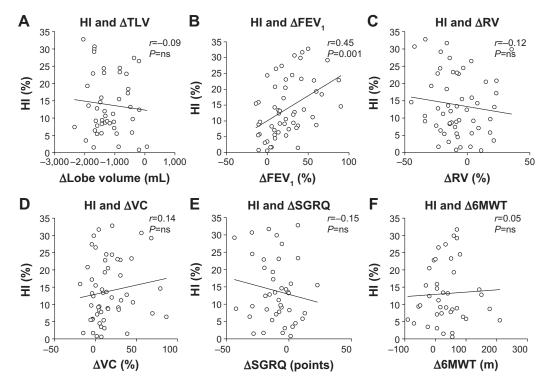


Figure S3 Correlations with baseline HI.

Notes: HI is the difference in emphysema scores between the potential TL and the ipsilateral lobe. *P*-values were calculated using the Student's *t*-test. (**A**) Correlation between HI and Δ TLV. (**B**) Correlation between HI and Δ FEV₁. (**C**) Correlation between HI and Δ RV. (**D**) Correlation between HI and Δ VC. (**E**) Correlation between HI and Δ SGRQ. (**F**) Correlation between HI and Δ 6MVVT.

Abbreviations: HI, heterogeneity index; TL, target lobe; △, change from baseline to follow-up; TLV, target lobe volume; *r*, Pearson's correlation coefficient; ns, not significant; FEV₁, forced expiratory volume in 1 second; RV, residual volume; SGRQ, St George's Respiratory Questionnaire; 6MWT, 6-minute walk test distance; VC, vital capacity.

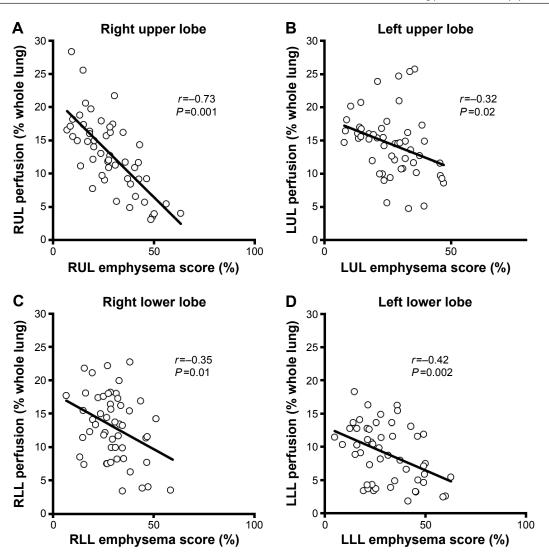


Figure S4 Correlations between baseline perfusion and ES for each lung lobe.

Notes: *P*-values were calculated using the Student's t-test. (A) Correlation between baseline perfusion and ES for the RUL. (B) Correlation between baseline perfusion and ES for the LUL. (C) Correlation between baseline perfusion and ES for the RLL. (D) Correlation between baseline perfusion and ES for the LUL. (C) Correlation between baseline perfusion and ES for the RLL. (D) Correlation between baselin

Reference

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